

Serial No.: 09/566,239

Filing Date: 05 MAY 2000

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PATENT APPLICATION/TECHNICAL DIGEST PUBLICATION RELEASE REQUEST

FROM: Associate Counsel (Patents) (1008.2)

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Via: (1) ⁷⁵Robert R. Whitlock (Code ~~6140~~)
(2) Division Superintendent (Code 6100)
(3) Head, Classification Management & Control (Code 1221)

SUBJ: Patent Application/Technical Digest entitled: "**TRANSMISSION CATHODE FOR X-RAY PRODUCTION**" Request for release for publication.

REF: (a) NRL Instruction 5510.40C
(b) Chapter 6, ONRINST 5870.1C

ENCL: (1) Copy of Patent Application/Technical Digest

1. In accordance with the provision of references (a) and (b), it is hereby requested that the subject Patent Application/Technical Digest be released for publication.

2. It is intended to offer this Patent Application/Technical Digest to the National Technical Information Service, for publication.

3. This request is in connection with Navy Case No. 79,348

5/25/00
(date)

BARRY A. EDELBERG
Associate Counsel (Patents)

FIRST ENDORSEMENT

Date:

FROM: Robert R. Whitlock (Code 6140)

TO: Division Superintendent (Code 6100)

1. It is the opinion of the Inventor(s) that the subject Patent Application/Technical Digest ~~is~~ (is not) classified and there is no objection to public release.

Robert R. Whitlock
Inventor's Signature

SECOND ENDORSEMENT

Date:

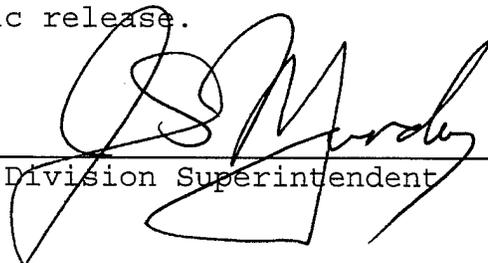
FROM: Division Superintendent (Code 6100)

TO: Classification Management & Control (Code 1221)

1. Release of Patent Application/Technical Digest (is) ~~(is not)~~ approved.

2. To the best knowledge of this Division, the subject matter of this Patent Application/Technical Digest ~~(has)~~ (has not) been classified.

3. This recommendation takes into account military security, sponsor requirements and other administration considerations and there in no objection to public release.



Division Superintendent

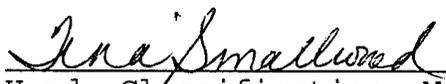
THIRD ENDORSEMENT

Date:

FROM: Head, Classification & Control (Code 1221)

TO: Associate Counsel (Patents) (1008.2)

1. This Patent Application/Technical Digest is authorized for public release.



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Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

TRANSMISSION CATHODE FOR X RAY PRODUCTION

BACKGROUND OF THE INVENTION

Field of the Invention

5 This device pertains generally to a device for generating X rays and more specifically to an X-ray transmission cathode wherein the X rays produced in an evacuated X-ray tube by an anode or sample are allowed to exit the tube through the cathode.

10 Description of the Related Art

 The typical configuration for a sealed X-ray tube involves a resistively heated, drawn wire filament cathode for generating free electrons in vacuum, and a metallic anode held at high voltage with respect to the cathode. The emitted electrons are
15 electrostatically accelerated to high energy and made to collide with the anode, which then emits the X rays. The voltages required for economical X-ray emission exceed the binding energy of inner electrons in the atoms of the anode, typically kilovolts. The anode emits continuum bremsstrahlung X rays as well
20 as characteristic X rays. Emission occurs in all directions, but the intensity in any direction is modified by the absorption of the X rays as they depart their points of origin. The characteristic rays are distinctive for each of the chemical elements, and form the basis of the well known elemental analysis

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

by X-ray emission. Selective detection, processing, and display techniques have been used to record the characteristic rays and analyze the spatial variations of composition in X-ray emitting materials.

5 As used herein, an x ray photon is a photon with sufficient energy to ionize a neutral atom by photoelectric absorption. There is a wide variation in the energy range of ionizing photons.

10 The usual geometry for sealed X-ray tubes **10**, as shown in **Figure 1a**, includes a filament cathode **12**, an anode **14**, and a separate X-ray "window" **16** made of thin material, usually metal, through which the X rays **18** exit the vacuum sealed X-ray tube **10**. It is well understood in the art that a fraction of incident x rays **18** are absorbed by any X-ray transmitting window **16** material
15 such as a window **16**, and that the suitability of a material as a window **16** is enhanced for smaller magnitudes of that fraction. The filament cathode **12** is connected between a pair of terminals **13** and **17**, to a cathode low voltage power supply **22** which supplies current to the cathode **12** to heat the filament cathode
20 **12** and excite electron flow **15**. A high voltage power supply **24** is connected to the anode **14** to accelerate the flow of the emitted electrons **15**. In this design, the anode **14** placement and shape is subject to two major geometric constraints, (1) maintaining sufficient distance between the anode **14** and other items that the

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

electric fields within the vacuum sealed X-ray tube **21** remain low enough to preclude breakdown and surface currents, and (2) insuring that the window **16** placement is such that X rays **18** are afforded sufficient solid angle to reach the outside of the vacuum sealed X-ray tube **21** with acceptable levels of absorption.

Typical vacuum sealed X-ray tube **10** design of the prior art places the sample or X-ray target **23** and window **16** such that X rays **18** are emitted at or near 90 degrees from the path of the incident electrons. Because X rays are less strongly absorbed than the electrons, angles are commonly chosen such that the electron penetration distance in the anode **14** is shorter than the exit path for emitted X rays **18**. X-ray **18** takeoff angles of 6 to 30 degrees (from the surface of the anode **14**) are not uncommon; appreciable X-ray absorption in the anode **14** occurs at these low angles.

A variant among tube designs of the prior art is the transmission anode, end window, tube **20**, as shown in **Figure 1b**, commonly known as the end-window tube, in which the transmission anode **26** functionalities of an anode and a window are combined in a single member. A transmission anode **26** must allow the electrons **29** to strike the anode **26** to produce X rays **31**, dissipate charge and heat from its surfaces and from throughout its volume, and permit the X rays **31** to pass through to the outside; these requirements are usually achieved with transmission anodes **26**

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

made of thin metal foils. The transmission anode, end-window tube
20 is advantageous in some applications, but the requirement for
a thin anode 26 results in lower X-ray 31 output power. It is
quite common for the end-window anode 26, an exterior component,
5 to be held at ground potential, which leads to the requirement
for the cathode 33 portion to be at high voltage. The cathode
filament current power supply 34 must float at high negative
voltage while the anode 26 is connected to a tube high voltage
power supply 32 to accelerate the flow of emitted electrons 31.

10 In contrast to tube designs of the prior art shown in
Figures 1a and **1b**, the transmission cathode, end-window, tube
discussed below, enables the X rays 31 from the transmission
cathode 33 to exit the anode 26 at the same angle that the
electrons 29 are incident, thus reducing the X-ray absorption and
15 enhancing tube 20 output and permitting grounded exterior
components. The transmission cathode 33 is not bombarded by high
energy electrons and need not dissipate as much charge or heat
from within its volume, thus it need not be as good a volume
conductor of either.

20 While the hot filament cathode based on thermionic emission
is very common, alternative technologies based on field emission,
photo emission, and plasma emission have been investigated as
well. Field emission tips have been used for X-ray production in
the past on radiography machines to produce nanosecond pulses of

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

X rays by accelerating electrons from an array of emitters into a metal foil end-window anode. Photoemission involves irradiating the cathode with suitable light sources capable of stimulating the cathode to emit electrons. **SEE**, U.S. Patent No. 5,042,058, Rentzepis, issued August 20, 1991, entitled ULTRASHORT TIME-RESOLVED X-ray SOURCE. Plasma emission cathodes involve locally heating the cathode surface to temperatures sufficient to produce a plasma, from which electrons are emitted. **SEE**, U.S. Patent No. 5,335,258, Whitlock, issued August 2, 1994, entitled SUBMICROSECOND, SYNCHRONIZABLE X-ray SOURCE.

Spatial resolution based on direct X-ray emission has been practiced with the electron microprobe and scanning electron microscope. Fluorescent X-ray emission has also been used for compositional mapping. **SEE**, U.S. Patent No. 5,742,658, Tiffin et al., issued April 21, 1998, entitled APPARATUS AND METHOD FOR DETERMINING THE ELEMENTAL COMPOSITIONS AND RELATIVE LOCATIONS OF PARTICLES ON THE SURFACE OF A SEMICONDUCTOR WAFER.

The focusing and collimation of arrays of micro electron sources has been well documented. **SEE**, US Patent No. 4,874,981, Spindt, entitled AUTOMATICALLY FOCUSING FIELD EMISSION ELECTRODE, and Cha-mei Tang ET AL.; PLANAR LENSES FOR FIELD-EMITTER ARRAYS; J. Vac. Sci. Technol. B **13**(2), Mar/Apr 1995, pp. 571-575.

Due to the unavailability of lenses for X rays, geometric imaging means are commonly used to generate X-ray images. X

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

radiography 30, as shown in **Figure 1c**, in which a sample 42 is imaged with X-rays 38, typically uses point projection imaging. A small ("point") source of X-rays 36 emits X-rays 38 spherically outward through the exit window of the tube (not shown). The sample 42 to be radiographed is placed between the X-ray source 36 and the imaging detector 44, e.g., an X-ray film plate used for medical imaging. The spatial resolution of the image is limited by the size of the X-ray point source 36. The achievable X-ray output power cannot exceed the ability of the X-ray tube 37 to absorb the heat load of its internal electron beam within the small focal point from which the X-rays 38 emanate. Where the sample is in close proximity to or contacting the imaging detector (typically X-ray film), the arrangement is called contact radiography and unit magnification is achieved. In typical applications where a magnified image is required, this can be obtained by moving the image plane further from the source and the image becomes a projection radiograph 45. This, in turn, increases the X-ray flux required to achieve an exposure, and places greater demands on the X-ray tube (not shown) and power supply.

Areal X-ray sources are not widely used for imaging, as the common filament cathode X-ray tubes are most conducive to providing small X-ray sources.

X-ray windows must transmit X rays, maintain vacuum

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

integrity as essential to the electron trajectories, and, if
needed, allow for the dissipation of charge or heat. The cathodes
taught in the prior art do not satisfy these requirements and are
insufficiently transmissive to X rays to permit their use as an
5 X-ray window.

SUMMARY OF THE INVENTION

The objective of this invention is to provide a device for
X-ray production wherein the X rays are transmitted out of the
10 device through the cathode.

Another objective of the invention is to provide an areal X-
ray source for X-ray fluorescence (XRF) system applications.

Another objective of the invention is to provide an areal X-
ray source for X-ray emission analysis applications.

15 Another objective of the invention is to provide an areal
cathode with addressable elements in an X-ray source for use with
a compositionally structured anode for the generation of tailored
X-ray spectra.

20 Another objective of this invention is to provide an areal
X-ray source for use with compositionally structured samples, for
use as an electron probe system.

Another objective of the invention is to provide an areal X-
ray source for use with compositionally structured samples, for
use with a collimator as an imaging electron probe system.

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

Another objective of the invention is to provide a cathode with addressable elements in an X-ray source for use with compositionally structured samples, for use as a imaging electron probe system.

5 Another objective of the invention is to provide a cathode with addressable elements for use with topographically or compositionally structured samples, for use as an scanning electron imaging system.

10 Another objective of the invention is to provide an areal X-ray source for use with a collimator for radiography applications.

15 These and other objectives are achieved by the use of a transmission cathode in an device for generating X rays. In the device an electrical current generated by a low voltage power supply produces an electron flow from the transmission cathode that is accelerated by a high voltage and propagates to an anode. As the X rays are emitted, a primary X-ray beam passes through the cathode striking a sample placed outside the tube. The transmission cathode is comprised of an electron emitter structure, preferably, a electron field emitter diode or 20 thermionic emitter or a photoemitter or a nanotube or a pyroemitter or a piezoemitter, fabricated, preferably of elements of atomic numbers of 14 (silicon) or below, with electrically conductive components or with conductive mechanical structural

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

components, preferably, conductive silicon or diamond or aluminum or beryllium metal, and non-conductive electrical insulators or non-conductive mechanical structural components, preferably, diamond or silicon dioxide or boron carbide.

5

BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1a shows a sealed, evacuated X-ray tube typical of the prior art.

10

Figure 1b shows an end-window, transmission anode tube typical of the prior art.

Figure 1c shows x radiography using point projection imaging with a point source X-ray tube, typical of the prior art.

Figure 2a shows a sealed, evacuated X-ray transmission cathode device as described in the preferred embodiment.

missing

15

Figure 2b shows a cross sectional view of a transmission cathode.

missing

Figure 2c shows a cross section of another transmission cathode.

20

Figure 2d shows the threshold voltage for a gatable diamond electron field emitter of the transmission cathode.

Figure 2e shows one manner in which the addressing of a selected row of gatable electron sources within an array of electron sources may be accomplished.

Figure 2f illustrates one manner in which the addressing of

individual gatable electron sources within an array of electron sources may be accomplished.

5 **Figure 3** shows a simple X-ray tube with an anode and a simple transmission cathode operating with an acceleration voltage.

Figure 4 shows components of a sealed, evacuated X-ray transmission cathode device with an array of cathode electron emitters, current supply, and accelerating voltage.

Duplicate figures

10 **Figure 5a** shows components of an evacuated X-ray transmission cathode device with circuitry to enable the electron source array to be gated and addressed in groups of electron emitters, and with a compositionally structural anode for producing tailored X-ray spectra, with particular application to X-ray fluorescence analysis.

15 **Figure 5b** shows a transmission cathode X-ray tube in use as a source of primary X-rays in an X-ray fluorescence system.

20 **Figure 5c** shows a transmission cathode X-ray tube in use as a source of primary X-rays in an X-ray fluorescence system in which the source and detector are designed for compact configuration. The transmission cathode X-ray tube is made in an annular shape, with the detector located on the axis of the annulus.

Figure 6a shows a miniature electron microprobe with a cathode as described in the preferred embodiment with array of

gatable electron emission sources that are individually addressable and may be scanned. Operation of the cathode in two-dimensional scanning mode allows a non-imaging X-ray detector system to record the sample spectrum at each illuminated point, and process the data as a two-dimensional scan to record the hyperspectral X-ray image of the sample.

Figure 6b shows deflection plates used to enhance imaging resolution, provide redundancy, and add control over beamlet impact point.

Figure 6c shows an imaging electron probe emission analysis system in which the sample is placed at the anode position of a transmission cathode X-ray tube, with image formed by an imaging X-ray optic such as a collimator, and detection of the X rays emitted by the sample being performed by an external imaging detector viewing the sample through the transmission cathode. The imaging detector records an image of the X-ray emission from the sample. Use of a spectral imaging detector allows the recording of the hyperspectral X-ray image of the sample.

Figure 6d shows an electron probe emission analysis system with an anode-window, through which electrons from the transmission cathode are accelerated to impact a sample located outside the sealed tube. X-rays emitted by the sample are transmitted by the anode-window and by the transmission cathode and detected by an X-ray detector. Scanning the transmission

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

cathode enables compositional imaging of the sample. X-ray emission may be detected from the front of any sample, or through samples that are sufficiently thin to transmit their own emitted X-rays.

5 **Figure 7** shows an X-ray probe emission analysis system, in which an anode-window of a scanning cathode tube is the source of primary X rays that may be used to radiograph or raster image a sample placed in close proximity. Alternatively, fluorescence emission from the sample may be used to image the sample.

10 **Figure 8a** shows a compact collimator X-radiography system with a large area, transmission cathode X-ray source. The collimator is disposed between the source and the sample, thus reducing the amount of x rays irradiating the sample.

15 **Figure 8b** shows a compact collimator X-radiography system with a large area, transmission cathode X-ray source. The collimator is disposed between the sample and the imaging detector.

20 **Figure 9a** shows a miniature scanning electron imaging system in which the sample is placed at the anode position of a tube having an addressable cathode array of gatable electron emitters. As each emitter is addressed in turn, scattered and other electrons originating from the sample or anode are collected by the unaddressed gate electrodes and recorded to form an image of the sample and anode. Alternatively, the sample current may be

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

collected and imaged in a similar fashion. Two-dimensional scanning is accomplished by addressing the cathode, and collimation is provided to the beamlets by electrodes on the cathode.

5 **Figure 9b** shows a cross section of a miniature scanning electron imager.

10 **Figure 10** shows a cross section of a miniature scanning electron imager with optional elements for controlling beam profile or beam deflection, or for retarding electrons emitted by sample or anode.

Figure 11 shows a variant construction for a diamond field emitter.

15 **Figure 12** shows a transmission cathode X-ray tube, monochromatic X rays from which are emitted in a beam of altered cross section by means of an asymmetrically diffracting X-ray optical element.

DESCRIPTION OF THE PREFERRED EMBODIMENT

20 In the preferred embodiment of the transmission cathode tube **30**, as shown in **Figure 2a**, an X-ray transmission cathode **46** is so designed that X-rays **48** produced within an evacuated, sealed X-ray tube **52** or pumped tube, are allowed to exit the tube **52** through the cathode **46**. The X-ray transmission cathode **46** emits electrons supplied by a low voltage power supply **54**. Electrons **56**

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

emitted by the transmission cathode 46 are accelerated by high voltage applied by a high voltage power supply 58 and impact the anode 62 to produce X-rays. The X-rays are emitted in all directions from the point of impact. X-rays 48 that strike the tube wall 52 are heavily absorbed. X-rays 48 that strike the transmission cathode 46 are transmitted and thus are emitted outside the tube 52.

Typical uses of an X-ray tube with transmission cathode 46 includes X-ray fluorescence (XRF) analysis, X-ray emission analysis, X-radiography (i.e., X-ray imaging), and X-ray diffraction. Further use of the scanning cathode array is found in the area of electron imaging systems.

A technologically simple configuration of known elements, combined to achieve a similar tube geometry, involves a free standing thermionic emission filament cathode disposed between an X-ray window and an anode. This device is distinct from all transmission cathode devices taught herein, in that the cathode (electron source) and window functionalities are not coalesced into a single item. The thermionic filament, which is operated at high temperature in proximity to the window, would quickly contaminate the window with evaporant and reduce its X-ray transmissivity. The filament cathode would produce a shadow image in the emitted X-rays, which would be of concern, for example, if it produced image contrast and fell within the imaging field of a

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

radiographic system or monochromatic beam used for diffraction.

The free standing filament cathode does not achieve the respective advantages taught below for transmission cathodes. The filament cathode is not an areal cathode, and does not achieve the respective advantages taught below for transmission cathodes.

In addition, the free standing filament cathode is not addressable, gatable, or scannable, and does not achieve these respective advantages taught below for transmission cathodes.

Referring to **Figure 2b**, the transmission cathode **46** is comprised of an electron emitter **64** structure, preferably, a film forming a diamond field emitter **66**, vapor deposited on a pre-molded structure on silicon forming a positive electrode **72** or on a thin insulating layer **68** approximately 1.0 μm thick, preferably SiO_2 on a conductive mold to shape the emitter tips **72** during processing, preferably microfabricated highly doped $\langle 100 \rangle$ silicon. **SEE**, Kang et al., "SUBVOLT TURN-ON VOLTAGE SELF-ALIGN GATE DIAMOND EMITTER FABRICATED BY SELF-ALIGN-GATE-SHARPENED MOLDING TECHNIQUE", J. Vac. Sci. Technol. B, vol. 17 no. 2, Mar/Apr 1999, p. 740-3. The diamond film **66** is intentionally deposited with a small component of sp^2 chemical bonding content. The silicon **72** mold is partially etched away to reveal the diamond emitter tips **74**. The heavily doped silicon mold **72** is used as the positive electrode of the electron emitter, that is, applying a positive potential to the silicon **72** with respect to

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

the diamond **66** results in electron emission by the diamond tips
74 into the space above the openings in the positive electrode.
The diamond field emitter **66** may be fabricated to a thickness and
geometry to provide its own support, in which case an additional
5 structural holder **64** is not required. However, other elements,
including metal conducting layers, doping layers, and other
electron emitter designs may be used in variant electron emission
designs, provided as they meet the criterion of being
transmissive to X rays. **Figure 2c** illustrates a novel
10 transmission cathode **40** with a metal layer forming the positive
electrode **402** of the electron emitter **404** .

Electron emitters of many types, including field emitters,
release electrons with a low energy per electron. This is
illustrated in **Figure 2d**, in which the threshold for emission by
15 diamond field emitters is presented. Diamond field emitters
without a surface treatment **74** are seen to require a higher value
of voltage per micrometer (and therefore a higher threshold
voltage) than do diamond field emitters that have undergone a
surface treatment **76**. The surface treated diamond field emitters
20 **76** have a desirably low threshold voltage. The low voltage at
which electrons are emitted by diamond field emitters and other
electron emitters allows the individual emitter to be gated on or
off by application of a suitable voltage to a gate electrode.

Referring again to **Figure 2c**, an above-threshold voltage may

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

be applied to all emitters **404** simultaneously causing them all to emit. By selectively applying an above-threshold voltage to certain emitters **404** and not others, the chosen emitters **404** may be induced to emit while the others do not emit. For example, in **Figure 2e** is shown an arrangement of gate electrodes **406** that permits a selected row of emitters **408** within the array of emitters **100** to be addressed and gated ON. A voltage, exceeding the threshold voltage, is applied to the selected row **408** and emitters **412** within that row **408** will emit electrons. Other arrangements or groupings of emitters **406** may be designed to be selectable, for example by hard wiring the gate electrodes **406** into arrangements or groupings or by controllably switching interconnections between gate electrodes **406**.

For the emitters **40**, as shown in **Figure 2d**, the change from nonemitting to emitting conditions occurs abruptly. For an applied gate voltage of half the threshold voltage, electron emission remains suppressed. In **Figure 2f** is shown an arrangement of gate electrodes **78** that permits individual emitters **82** to be addressed and gated on. Two gate electrodes **78** are disposed above each addressable emitter **82**. The gate electrodes **78** may be electrically connected in rows **84** and columns **86**, as depicted in **Figure 2f**. The rows **84** are separated from one another laterally by an insulating surface **92**, and the columns **86** are separated from one another laterally by another insulating surface **88** which

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

is depicted for convenience in illustration to be also the transmission cathode substrate 88. A sub-threshold voltage 85, less than the threshold voltage, is applied to each of the two gate electrodes 78 disposed above the desired emitter 82. The
5 desired emitter 82 experiences a net voltage at or above the threshold, and emits a beamlet of electrons. The gate electrodes 78 of adjacent emitters 82 may also receive a voltage, but only one gate electrode 78 will experience a voltage at any emitter 82 other than the desired emitter, and thus only the desired emitter
10 will exceed threshold. (Other geometric arrangements of a plurality of gate electrodes may be applied at each emitter 82, for example, three electrodes 78, with the adjacent electrodes 82 being electrically connected in lines at 60 degree angles instead
lines at 90 degree angles. Other addressing means may be
15 employed, such as individually wired gates addressed by switching circuitry. Collimation and focusing of the beamlets may be achieved by suitably shaping the gate electrodes or by addition of supplementary electrodes.

The concept of gating and gate voltage, as used herein,
20 includes binary switching OFF and ON. However, for emitters that increase output currents as gate voltage increases, the gate voltage provides a means for controlling the magnitude of the current. Thus, gating includes the capacity to exercise such control.

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

5 Features on the microfabricated cathodes **40** may be made of any suitable material, as dictated by the functionality required. For example, aluminum or other metal conducting paths or layers are admissible. The physical thickness of such conducting paths is very small, and the resultant X-ray absorption in them is not great locally, and even lower when averaged over the entire area of the cathode **40**. Thus enhanced functionality can be acquired by adding structures of higher atomic number, while retaining a usefully low value of X-ray transmission through the full aperture of the transmission cathode **40**.

10 There is a wide range of techniques for treating surfaces, processing materials, and fabricating structures, operating on length scales from the nanometer scale to the macro scale, which may be applied to the transmission cathode tube **40** or its components. These are well known to those skilled in the art.

15 The transmission cathode substrate **88** or window material may be any X-ray transmissive material satisfying the criteria set forth herein and durable to X-ray irradiation, such as thin metal, polyimide, nitrides, carbides, diamond, or silicon. Particular advantages may be achieved with substrates made of elements in the low atomic number range of 1 and 14 (hydrogen through silicon), due to the lower X-ray absorption, per atom, of low atomic number elements, and the fact that their absorption edges fall well below the energies used in most practical X-ray

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

work.

Many advantages are inherent in the use of electron emitters having closely placed electrodes to perform the functions of electron extraction or gating. One of these advantages is the low voltages which may be applied to achieve the extraction or gating functions, a particularly important issue for devices controlled by solid state electronics. However, in X-ray applications for which high voltages are required to stimulate x ray production, it is not always required to employ low voltages or to incorporate these closely placed electrodes in order to achieve X-ray emission. **Figure 3** illustrates a fundamental X-ray tube configuration of a simple transmission cathode **414** and an anode **416**, held in an environment suitable for electron **418** transit between the cathode **414** and anode ~~**418**~~^{**416**}. The transmission cathode **414** may be, for example, all diamond on which diamond emitter tips **415**, or other types of electron sources, are formed as before but without overlays to form extraction or gate electrodes. Or, emitter tips **415**, formed of any material that performs as an emitter, may be placed on an electrically conductive, X-ray transmissive substrate ~~**414**~~^{**417**} and occupying a fraction of the total area of that substrate. The emitter tips **415** may be made of the same material as the substrate **417**, if that material performs as an emitter. This combination of emitter tips **415** and substrate **417** forms a transmission cathode **414**. For

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

sufficiently close spacings between emitter tips 415 and anode 416, the application of high voltage between the cathode 414 and anode 416 is sufficient to enable electron emission. Emission current may be gated by removing either the high voltage or the
5 current supply. Emitted electrons 418 are accelerated to the anode 416, where they produce x rays 421. Emitted x rays 421 may transmit through the transmission cathode 414 and escape the X-ray tube 423.

10 In further detail of the cathode and anode arrangement of the preferred embodiment of the transmission cathode tube 50, as shown in Figure 4, an X-ray transmission cathode 92 with electron emitter array 94 is so designed that X rays 96 produced within an evacuated sealed X-ray tube, or pumped tube (not shown), are allowed to exit the tube (not shown) through the cathode 92.

15 An electrical current generated by a low voltage power current? supply 104 produces an electron flow 106 from the transmission cathode 92 that propagates to the anode 108 which is impacted by an array of overlapping beamlets at beamlet impact locations 114. As electrons 106 strike the anode 108 X rays 96 are generated
20 that pass through the cathode 92 and exit the tube (not shown).

The electron flow 106 from an individual electron emitter or an array of individual electron emitters 94 on the cathode is accelerated towards the anode 108 by a high voltage from a power supply 112. X rays 96 are generated in all directions from the

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

anode 108. The X rays 96 that strike the walls of the tube (not shown) and are heavily absorbed. The theories of X-ray emission and absorption are well known to those skilled in the art.

5 The transmission cathode 92 may use a thermionic, field, photo, pyroelectrically stimulated, piezoelectrically stimulated, or plasma emission to generate the electron current within the tube (not shown). In order to qualify as a transmission cathode 50, the X rays 96 need only to be able to exit through the cathode 92 in sufficient quantity to be of use. The transmission
10 cathode 50 may include features covering a part of its area which heavily absorb X rays, so long as the transmission through the remaining cathode 92 area remains sufficient to be useful. Features on or in the cathode 50 may be fabricated of material of any atomic number or combination thereof. The cathode 50 may also
15 include surface coatings, for example to provide a conducting path to drain away surface charge, or dopings, for example to control bulk conductivity.

20 Unlike the end-window tube, the transmission cathode 50 may be used with a thick anode 108, which improves X-ray 96 production efficiency compared to thin anode X-ray production. The near normal angles of X-ray emission 96 attainable from transmission cathodes 50 offer less absorption than is typically experienced with thick target, side window geometries having the common non-transmission cathode. The transmission cathode 50 may

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

be held at ground potential which simplifies the electronics (not shown) required to supply current and acceleration potentials to the cathode 50. As the transmission cathode 50 is a component of the tube (not shown) externals, it is desirable from a safety
5 standpoint for it to be at ground potential.

In another preferred embodiment 60, as shown in **Figure 5a**, for producing tailored, variable X-ray spectra, the transmission cathode 116 in the device 60 is defined in regions of electron sources 117, each of which may be gated ON or OFF. Each cathode
10 region 117 impacts a different respective anode region 118. For convenience in illustration, the regions 117 and 118 are shown as rectangles, although other shapes may also be used. The compositions of the anode regions 118 are variously fabricated to
15 irradiating a sample 122 with X rays 124 of varying wavelengths.

As the energy of emitted electrons 128 is initially low in thermionic, field emitters and photo emitters, individual electron sources of these types in the emission arrays 118 may be electrostatically gated by using low voltage 126 gating near the
20 electron source; only those sources that are gated on will produce electron beamlets which pass into the region of the tube where the electrons will be accelerated to high voltage and produce x rays. The individual electron sources 117 of the array may be made to be switched ON or OFF, or to emit a variable value

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

of current, as discussed above, in relation to field emitter
electron sources. The low extraction voltages **126** allow control
by control circuitry **136**, and thus enable the electron array
source in the transmission cathode **116** to be addressed and
5 scanned; the X-ray emission **125** from the electron target can thus
be scanned under control of circuits **136**. Methods and techniques
of vacuum microelectronics have been published by others for use
in electron devices. Here is taught their use for X-ray
production and X-ray imaging.

10 Plasma electron sources are capable of emitting much more
energetic electrons, depending on the plasma conditions. Gating
of plasma emitters will require gating voltages commensurate with
the energy of the emitted electrons. The degree of cathode mass
erosion to which plasma sources are susceptible is a disadvantage
15 not shared by the other methods, and limits the practical uses of
plasma emission sources.

An areal cathode **116** with multiple areas of gatable
electron emission sources **118** and respective anode compositions
will be useful for spectrographic applications such as X-ray
20 fluorescence analysis.

A low-voltage power supply **126** applies a voltage to the
cathode **116**, as described above, generating an electron beam or
flow **128** that is accelerated by high voltage **132** to an anode **134**.
The anode **134** is specifically fabricated with different known

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

5 compositions at different known locations. The anode 134 is
comprised of various known segregated elements 118, such as
copper, iron, aluminum, tungsten and molybdenum, or alloys or
compositions that, when struck by the electron beam 128, radiate
X rays 124 of varying frequencies which propagate to the sample
122 through the cathode 116, as described above. The X-ray
spectrum from each location will differ with the composition. The
compositional variations may be designed to the micrometer scale
or larger. The various areas forming the cathode 118 may be
10 switched ON and OFF by a control circuit 136 to select the
desired respective area of the anode 118 that will be struck by
the electrons 128 to generate the X-ray wavelength desired.
Although a list of elements has been enumerated above, other
elements may also be used, this is a teaching that is well known
15 to those skilled in the art. In applications where a single
tailored spectrum is desired without variation, the
compositionally varied anode 134 may ^{be} manufactured to provide the
desired spectrum when irradiated by emitters 117 that need not be
separately gated.

20 The fields 128 between the cathode 116 and anode 134
determine the size and point of impact of the beamlet, and thus
determine the X-ray source location and size attributable to that
beamlet. The electron optics are optionally so that adjacent
beamlets are essentially contiguous, overlapping, or separate. A

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

single beamlet strikes the anode **134**, producing X rays **124** which exit the tube through the transmission cathode **116**. This process is repeated in succession, or concurrently, with other beamlets. The location of the X-ray sources for each beamlet is known from the geometry of the components including the cathode **116** and electron optics (not shown). The elemental composition of each successive anode source point **118** is known by design. The total X-ray spectrum is the sum of the spectra from the various source points. The anode **134** may contain multiple points of the same composition. The spectral contribution of a particular composition may be enhanced by gating on more points of that composition, or by gating them on for longer periods of time.

The primary X rays **124** emitted by the transmission cathode tube **60** irradiate the sample **122**, which fluoresces according to well known physics. The fluorescence X ray **138** is detected by a spectral detector **142** whose output is captured by an analysis system, typical of those known in the art of X-ray spectral detection systems, and spectrally analyzed by computer to determine the chemical elemental composition of the sample.

Spectral measurements are performed by the spectral detection system **142**. The spectral detection system **142** may be an energy dispersive (ED) detection system or a wavelength dispersive (WD) system. WD apparatus disperses the X rays in space, each wavelength to a different angle, using X-ray diffraction, e.g.,

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

from a crystal or multilayer. The detector in a WD apparatus need only count the number of photons arriving, as the wavelength is known from the angle at which the diffractor is tuned.

5 ED apparatus absorbs individual X-ray photons, converts the photon to an electrical pulse, quantifies the number of electrons in the pulse, and relates the pulse amplitude to photon energy. Photon energy E and photon wavelength W are related by the simple relationship $EW = \text{constant}$, where the value of the constant is well known (12.398 for E in kilo electron volts (keV) and W in
10 Angstroms). Due to the mechanical simplicity of ED systems and their suitability for digital data capture, they are preferred in all but the most demanding work. The spectral measurements made by the detection system 142 are analyzed by a computer (not shown) to determine chemical elemental composition, using methods
15 well known to those skilled in the art.

The function of an XRF system is to irradiate a sample with X rays to stimulate the sample to emit its own fluorescent characteristic X radiation 148. It is advantageous for XRF analysis to be able to vary the primary X-ray spectrum
20 illuminating the sample. At present, this is typically accomplished by irradiating the sample 144 with fluorescent x rays 148, by use of x ray filters ~~144~~ or 147, or by replacing the entire X-ray tube with one having a different anode material. A tube with tailored spectrum would obviate the need to rely on the

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

lower intensity of fluorescence or filtered sources, and it would no longer be necessary to replace the tube simply to alter the spectrum.

5 In another preferred embodiment, X-ray fluorescence (XRF) systems employing transmission cathode X-ray tubes 70 and 80 , as shown in **Figures 5b** and **5c**, may differ in the placement of the detector 142. The transmission cathode X-ray tubes 70 and 80 may have single or multiple composition anodes 146. **Figures 5b** and **5c** show two typical optional placements of the detector 142; only
10 one detector 142 is necessary in a given system. **Figure 5c** shows a side view of an annular areal transmission cathode X-ray tube 80, from the center of which the detector system 142 views the sample 144.

15 In XRF systems, areal X-ray sources are advantageous because greater X-ray power can be achieved by applying the heat load to a larger area of anode, enabling higher total output X-ray power. XRF systems do not require spatial resolution, so a small source is not required. The areal transmission cathode X-ray tube achieves these advantages.

20 A transmission cathode tube may be configured to operate as an electron microprobe 90, as shown in **Figure 6a**. An electron microprobe is a large laboratory instrument similar to a scanning electron microscope (SEM) that scans a beam of energetic electrons onto micrometer areas of a sample to produce

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

characteristic x rays that are detected by a non-imaging spectral
detection system. These characteristic X rays are not fluorescent
X rays, for fluorescence results from photon (i.e., X ray)
excitation not electron excitation. However, the X-ray emission
5 wavelengths are the same in the two cases, so the detection and
analysis subsystems may be identical to these used for XRF. Both
methods of excitation are useful for the spectral determination
of chemical elemental composition. The emitted characteristic X
rays may be detected by an ED or WD X-ray detection system and
10 analyzed to determine the chemical composition of the sample, as
with fluorescence x rays. Electron probe imaging has become so
popular that X-ray detection attachments are commonly found on
laboratory SEMs. Contemporary electron microprobes have higher
electron beam currents than typical SEMs, and likely also have a
15 larger focal spot on the sample.

A conductive sample **152** that withstands vacuum conditions
may be placed in the anode **154** position of a transmission cathode
X-ray source **90**. X rays **156** emitted by the electron-irradiated
sample **152** are detected by an external, non-imaging, spectral
20 detector **158** viewing the sample through the transmission cathode
162. For a system with a gatable and addressable transmission
cathode **164**, the image of the sample **152** and anode **154** is
acquired by scanning the cathode array **162**. The compositionally
structured anode **134** is now the sample **152** in **Figure 6a**, and

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

gating is performed on small groups or individual electron emitters 164 in **Figure 6a** rather than on regions or larger areas of emitters 117 as in **Figure 5a**. The X-ray detector 158 is located outside the probe 90. Either ED or WD detection or both
5 may be used. (The entire sample 152 may be compositionally analyzed at once but without spatial imaging by activating all electron emitters 164 simultaneously in area illumination.)

A gatable and addressable transmission cathode 162 may be scanned. Successive electron emitters 164 are scanned, each
10 producing an electron impact point on the sample 152 or anode 154, X rays 156 emitted by the electron impact 154 point are recorded digitally in a computer 168 as an image. When a spectrum recording detector is used, the recorded image is an array of spectra known as a hyperspectral image cube. The image cube may
15 be analyzed and displayed as a compositional map of the sample on a computer monitor screen 172; various mappings are possible for a sample containing multiple chemical elements. A single detector 158 may measure many or all X-ray 156 source points in succession. Multiple detectors 158 may view the source points to
20 achieve particular additional advantages. For example, different X-ray filters (not shown) may be applied to the different detectors 158, or different types of detectors 158 with differing response characteristics may be employed as an aid to enhancing the quality or speed of data acquisition.

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

The imaging granularity of the scanning electron microprobe 90 will be limited by the spacing between emitters in the cathode array 162. While this spacing is larger than the resolution achievable with large, laboratory sized instruments, the simplicity of construction, small size, and suitability for microfabrication offer significant advantages for particular applications which the large and costly laboratory sized instruments cannot meet.

In another preferred embodiment, as shown in **Figure 6b**, the image granularity of the scanning electron microprobe 100 may be reduced by the addition of elements, such as electrostatic deflection plates 174, to control the scan of the electron beamlet 176 over distances less than the spacing interval. An electron beamlet 176 may then be placed controllably on intermediate points on the sample 178, between the home impact areas that adjacent beamlets 176 would impact if no deflection were applied. For example, electrostatic deflection plates 174 may be used to scan a deflected beamlet 176 onto the home impact area that its neighbor beamlet would impact if no deflection were applied. Deflection plates 174 may be placed so as to deflect all beams that may be transiting the tube 100. By varying the deflection voltages 182, the deflected beamlet 176 can be made to strike its own home impact area, that of its neighbor, or any intermediate point, whereby finer positioning than the source

spacing is achieved. In addition, redundancy is achieved, whereby the same area of sample 178 may be addressed by neighboring beamlets in succession by use of deflection circuitry applied to the deflection plates 174 and gate and scan control circuitry 184 applied to the transmission cathode 186.

In another preferred embodiment, as shown in Figure 6c, multiple source points of a collimator imaging probe system 110 may be activated simultaneously. The sample 186, in the anode 188 position, is again illuminated directly by electrons 192 to generate characteristic X rays 194 from the sample 186. The collimator 195 preserves the X-ray emission image of the sample 186 onto an imaging detector 196. A spectral imaging detector may also be used to collect a hyperspectral image cube.

In another preferred embodiment, as shown in Figure 6d, having a scanning transmission cathode with anode-window electron probe 120, where an anode 198 is fabricated having sufficiently thin regions, or fabricated of a sufficiently thin material such as thin beryllium metal foil, the electrons 202 may be accelerated from the cathode through the anode 198 and into an external volume containing a sample 206. The transmission cathode 208 and electron optics (not shown) may then be completely sealed and maintained clean of possible outside contaminants. The sample 206 is placed close to the anode-window 198. The volume holding the sample 206 may be evacuated to facilitate electron 202

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

transit to the sample 206, while retaining the benefits of a sealed source tube 204. Alternatively the volume holding the sample 206 may be filled with a low density or low atomic number gas. The transmission cathode 208 may be scanned or activated on an areal basis using a gate and scan control circuitry 218, as in
5 the previous examples. X rays 214 emitted by the sample 206 are transmitted through the sample 206 holding volume, through the anode-window 198, through the transmission cathode 208, and detected by a first detector 216. Also X rays 212 emitted by a
10 sufficiently thin sample are transmitted to a second detector 222. Scanning the transmission cathode 208 can be used to image the composition of the sample 206, as before, using a first detector 216 or a second detector ~~232~~ 222

In another preferred embodiment, an X-ray probe tube 130, as
15 shown in **Figure 7**, is outfitted with an anode-window 226 of higher atomic number (Z) and greater mass thickness, an X-ray probe may be produced. The probe 130, includes a scanning transmission cathode 228 and the higher Z anode-window 226 in an evacuated, sealed or pumped tube 244. As the electron beamlets
20 232 scan across the anode-window 226, the anode-window 226 emits primary X- rays 234 from successive impact points. The scanning is controlled by the use of gate and scan control circuitry 252. The scanned anode-window 226 becomes a scanned X-ray source.

A sample 236 placed in close proximity to the anode-window

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

226 may also emit characteristic fluorescent radiation in all directions and may be viewed by variously placed X-ray detectors. Fluorescent X rays 248 from the sample 236 that transit through the anode-window 226 and through the transmission cathode 228 may be detected by a first detector 238. Fluorescent X-ray emissions 245 from the sample 236 may be viewed in transmission through the sample by a second X-ray detector 246 in the Sample Transmission position. More highly absorbing portions of the sample 236 will present weaker transmitted fluorescent X-ray signals 245 to the second detector 246. Alternatively, an areal imaging detector (not shown) may likewise be placed in close proximity to the sample 236 to receive and, by collimator or contact radiography, record the X-rays 245 transmitted through the sample 236 to the areal imaging detector.

Both detectors 238 and 246 will also view the anode-window 226 source. Much of the intensity of unwanted X rays 242 from the anode-window 226 source may be reduced for the Sample Transmission detector 246 by moving the detector 246 off axis, as shown, and interposing a suitably fine collimator (not shown) between the anode-window 226 and the sample 236.

In an arrangement not shown, the transmission cathode X-ray source may be used in point projection radiographic imaging systems. For radiographic systems, a small X-ray source (not shown) is often preferred to the use of collimation. The usual

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

requirements on X-ray source size and placement apply. The compactness of the transmission cathode X-ray source (not shown) may offer significant advantages. To meet this need for a point source, the areal cathode's **274** electron current can be focused ^{in Fig. 8a} to a small area on the anode **276**, using additional whole-beam focusing elements (not shown) to shape the fields within the tube (not shown), as is well known to those skilled in the art of electron focusing. The limitations on X-ray power delivered by point source X-ray tubes (not shown) are set by the temperature at which the anode **276** metal vaporizes or melts. The lifetime of the common filament tube is often determined by the lifetime of the filament. The areal transmission cathode **274**, with convergent electron beam geometry to produce a point focus, offers redundancy in the electron source, extended cathode **274** life and thus greater tube life.

In another preferred embodiment, as shown in **Figures 8a and 8b**, an areal transmission cathode X-ray tube **140** and **150**, respectively, used for X-radiography, performs the function of graphically imaging a sample with X-ray illumination, e.g., a chest X-radiograph. Because an image is formed, an imaging detection system **254** is required. Areal X-ray sources are infrequently used in radiographic imaging systems. Areal sources require collimation to refine the image resolution. An X-ray collimator **272** is analogous to venetian blinds, allowing view for

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

some angles but not for others. X-ray collimators **272** are made in various geometries. Soller slits are a stack of planar absorbing sheets separated by open spaces through which X-ray transmission is permitted. Tube collimators **272** are a stack of tubes; X rays
5 pass through the centers of the tubes and in the open spaces between tubes. Square cylindrical tubes are also used for X-ray collimation, as are hexagonal structures. The basic concept with collimators **272** is to make the acceptance angle of the collimator **272** sufficiently small that the image is resolved, but as large
10 as permitted so as to retain as much X-ray flux **268** as possible.

Three key features of collimators **272** for X-ray imaging are (1) collimators **272** function by absorbing X rays **268**, (2) collimators **272** require areal sources to be effective for imaging, and (3) collimator **272** imaging arrangements can be very
15 compact. X-ray sources of large enough size to be of interest for compact collimator **272** imaging have not generally been available. X rays **268** absorbed by the collimator **272** are of no value, and the power used in producing them becomes lost power. Here, the salient parameter is local source brightness more than total
20 output power. For these reasons, collimators **272** are rarely used for imaging.

The transmission cathode **274** makes large area X-ray sources a possibility, and therefore makes compact collimated X-radiography a possibility. Losses due to X-ray **268** absorption in

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

the collimator 272 remain an issue, as does the brightness of individual source elements. A collimator X-ray imaging system ~~150~~¹⁴⁰ and ~~160~~¹⁵⁰ with an areal transmission cathode source 274 can achieve constant incident intensity across a large sample 262 to be imaged in a compact arrangement.

The collimator 272 for the X-ray source may be located in any of several possible locations. Figure 8a shows the collimator 272 between the transmission cathode tube 274 and the sample 262. In Figure 8b, the collimator 272 is shown between the sample 262 and the imaging detector 254. The collimator 272 may also be included within the X-ray tube (not shown).

In another preferred embodiment, as shown in Figure 9a, a scanning electron imaging system 160 in which the sample 278 is placed at the anode 282 position of an evacuated tube 284 has an addressable cathode array 286 of gatable electron emitters 292. Control of the gating of the gatable electron emitters 292 is provided by the use of circuitry for gating and scanning, according to techniques that are well known to those skilled in the art. The electrons 302 emitted by the cathode 286 are primarily electrons. As each emitter 292 is addressed in turn, scattered and other emitted electrons 294 emanating from the sample 278 or anode 282 are collected by electrodes within the tube 284 utilizing circuitry for collecting sample 278 scattering and emission current within the tube 284, for example the

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

unaddressed gate electrodes 286, and recorded to form an image of the sample 278 and anode 282. Regions of the sample 278 that cause many electrons 302 to be collected will appear differently in the image than regions that cause few electrons 302 to be collected. Compositional as well as topographic variations are known to influence electron scattering and emission by the sample 278. Additional or alternate electron 302 collection means may be implemented. Alternatively, the sample current may be collected and imaged in a similar fashion. Sample current is that part of the primary electron current 246 that is collected by the sample 278 or anode 284. The accelerating voltage of the emitted cathode electron beamlets 302 may be greater than or less than the voltages required for an X-ray emitting tube. For lower accelerating voltages, the sample 278 may optionally be placed closer to the cathode array 286. The X-ray transmission properties of the cathode 286 are not of concern for the operation of this tube as an electron imaging system. This system requires no magnetic lenses for focusing and no deflection electrodes to accomplish raster scanning. Raster scanning is accomplished by addressing the cathode, and collimation is provided to the beamlets 302 by the gate electrodes 292 or other electrode structures as is well known to those skilled in the art. An electron imaging system 160 is thereby achieved in a device with simplicity of design, manufacture, and use.

In **Figure 9b**, a cross section of a miniature scanning electron imager **170** is depicted in which additional elements are added for the purpose of enabling or improving the detection of electrons **442** from the sample **418**. The cathode **424** may be either
5 absorbant or transmissive to x rays. The gatable electron sources **425** may be any of various varieties of electron sources, including field emitters, photoemitters, thermoemitters, or other types of electron emitters. Individual emitters or groups of emitters are gated sequentially. For purposes of illustration,
10 multiple beamlets **422** of electrons are emitted by the electron emitter **425** under control of electron source gating and control circuitry **423**. The beamlet ~~427~~⁴²² electrons are accelerated toward the anode **428** and a sample **418** by high voltage **432** in an evacuated enclosure ~~432~~⁴³³. The beamlets ~~427~~⁴²² impact a sample **418** or
15 the anode **428** to produce secondary electrons emanating from the sample or anode, and some of the incident electrons in the beamlet **422** are backscattered ~~420~~⁴²⁷ by the sample or anode. Some of the secondary electrons and back scattered electrons are collected or detected by electron detectors **426**. The signals from
20 electron detectors **426** are received and processed by electron detector circuitry **434** to form an electron image of the sample **418**. The electron detectors **426** may be any of various varieties of electron detectors well known to those skilled in the art.

Additional elements may be added, singly or in combination,

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

to provide improved electron detection or improved electron beam handling or both, such as in a miniature scanning electron imager **180**, as illustrated in **Figure 10**. Devices for electron collection and detection may be added as shown, whether on existing
5 substrates or on new substrates or holders, and placed in a manner not to impede the primary electrons or beamlets **428** but to collect the electrons **802** back scattered or secondary electrons emanating from the sample **432** or anode **434**. These devices for electron collection and detection may rely on scintillation, or
10 direct charge collection performed by devices such as silicon devices or Faraday cups or conducting electrodes, or may rely on electron amplification performed by devices **438** such as electron multipliers, channel electron multipliers, microchannelplates, and the like. The electron collection and detection devices **438**
15 are connected to electronics for processing the detected signal. The electron collection and detection devices **438** may have the facility to accelerate or decelerate electrons **436** from the sample **432**, by application of suitable voltages to the devices themselves or to electrodes or screen grids **436** or the like
20 placed between the devices **438** and the sample **432**. Additional elements **804** may be optionally added for controlling the beamlet **428** beam profile, such as ring shaped electrodes, hollow cylindrical conducting electrodes, or other elements of shapes well known to those skilled in the art of electron optics to be

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

effective for controlling beam **428** profile by means of electric fields, or such as magnet coils or magnets for controlling beam profile by means of magnetic fields. Further elements **806** for controlling the deflection of individual or multiple beamlets
5 **428**, with associated deflection electrical control circuitry, may be optionally added as illustrated in **Figure 10**. Provided the cathode **442** of the imager **180** of **Figure 10** is a transmission cathode, the imager **180** may further be used as an electron microprobe when outfitted with X-ray detection.

10 It is to be understood that elements for controlling beam profile or beam deflecting or electron collectors or electron detectors, described here with reference to a scanning electron imager, may optionally be incorporated into an electron probe image analysis system **90**, as in **Figure 6a** or an X-ray probe
15 emission analysis system **130**, as in **Figure 7**.

In a preferred embodiment of the variant transmission cathode, a different diamond electron field emitter **190** may be employed as a transmission cathode, as shown in **Figure 11**. See, Normile, FIELD EMITTERS FINDING HOME IN ELECTRONICS, Science,
20 Vol. 281, pp. 632-633, 31 Jul 98 and Kang et al., ULTRALOW BORON-DOPED DIAMOND FIELD EMITTER VACUUM DIODE, Elect. Dev. Ltrs., Vol. 19, No. 10, pg. 379, Oct. 98. A cover device **296** of silicon, on layer of silicon oxide **304** which has been deposited on a glass substrate **306**, encompasses a diamond emitter diode **298** and over

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

each diode 298 is an opening 302 to allow passage of electrons 301 to the anode 303. In other designs, metal gate electrodes are used as positive electrode for field extraction and collimation of the electron beam. Other types of field emitters, not
5 involving diamond, may also be used in transmission cathodes.

The ability to make micro-heaters has been amply demonstrated in the microelectronic mechanical systems (MEMS) teachings. Arrays of such micro-heaters can be used as thermionic electron sources, with total areas much larger than the area of a
10 typical drawn filament. Micro-heater thermionic electron sources may be switched by controlling the heater currents for each source. Electrostatic switching of the emitted electrons remains as an available switching option which may be implemented. Two
15 emission controls are then available: heater current and gate potential. Electron emitters based on thermionic emission may be used as electron emitters in transmission cathodes, or in electron imaging, as taught herein,

A hybrid approach could use field emission aided by moderately elevated temperature, i.e., significantly lower
20 temperature than those at which drawn wire filaments are typically operated, yet above the ambient. This hybrid approach removes some of the disadvantages of high temperature. As above, two parameters are available for controlling beamlet current, namely emitter potential and emitter temperature.

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

A photoemitting cathode may be used, which includes a suitable substrate holding a photomissive material on its surface inside the X-ray tube. The substrate may be monolithic. A light source is arranged to illuminate the photoemitter with

5 sufficiently energetic photons as to stimulate electron emission. As X rays are themselves sufficiently energetic photons as to stimulate photoemission, even from metallic surfaces, the emitted X rays will aid in the continued operation of the device, provided they impinge on photoemitting material. By using a

10 microchannel plate electron multiplier in conjunction with the photocathode, the X rays absorbed by the cathode (or microchannel plate) can stimulate electron emission which will supply the anode with sufficient emitted electrons to maintain a self-sustaining X-ray intensity on the cathode. The emission may be

15 ceased by removing the high voltage or restricting the cathode current, thus preventing the electrons from reaching X-ray emitting energies. Electron emitters based on photoemission may be used as electron emitters in transmission cathodes, or for electron imaging, as taught above.

20 In a micro-photoemitter array design in which the photoemissive material is patterned on the cathode in an array geometry, the array elements may be selected and gated on by virtue of their being illuminated by photons. Alternatively, the emitted electrons from photoemitters may be electrically gated as

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

with other methods of emission. In yet another alternate, each array element may incorporate a photoswitch which, upon illumination, causes a gate voltage to be applied to the respective electron emitter, which then emits. Selection or scanning of individual elements or areas can be performed by illuminating or masking of photoswitches that apply gate voltages.

Other elements, including metal conducting layers, doping layers, and other electron emitter designs may be used in variant electron emission designs. For transmission cathodes, the resulting structure must meet the criterion of being transmissive to X rays. The various electron emitters disclosed for transmission cathodes may also be applied for electron imagers and X-ray probes.

The use of areal electron emission from an array of electron emitters reduces the current requirements on each electron source. The current requirements are closely linked to longevity and reliability; thus, the disclosed cathodes offer the potential for increases in both.

A recent technology for electron emission is offered by microfabricated devices. Small cross section microstructures including electron emitters can be fabricated directly on or spanning small gaps on various substrates, such as silicon or others. Microfabrication can be carried out with virtually any

Inventor: Whitlock et al.
Serial No.

PATENT APPLICATION
Navy Case No. 79,348

class of material, including metal conductors, insulators, or semiconductors. Each micro electron source produces a beamlet of electrons. Microsources can be arranged in arrays or formed in patterns of any suitable shape.

5 X-ray diffraction applications typically make use of only small angular segments of the x rays emitted by X-ray tubes. This is a natural consequence of the small range of incident and reflected angles (typically much less than a degree of arc) over which the conditions are satisfied for X-ray diffraction by
10 optics such as crystals. This, combined with the relatively small source size of X-ray tubes, leads to the restriction that diffracted X-ray beams are low power and small. The small size of diffracted beams has been addressed by Boettinger, et al., who taught a method of using asymmetric diffraction to expand the
15 cross section of a diffracted beam to sizeable and useful extent, with an associated lowering of the power per unit area of the beam. (SEE W.J. Boettinger et al., X-RAY MAGNIFICATION, Rev. Sci. Instrum., Vol50, No. 1, pp.26-30, 1979). Alternately, the Boettinger technique can be used in reverse to reduce the cross
20 section but increase the power per unit area of the beam. One crystal is required for each dimension in which an X-ray beam size alteration is to be carried out. Any diffractor from which asymmetric diffraction may be produced can be used in a Boettinger arrangement.

In another preferred embodiment, as shown in **Figure 12**, 200
the areal transmission cathode tube **502** offers a means for
producing X rays from a large area. The total power emitted from
an areal transmission cathode tube **502** can exceed the power
5 available from a standard X-ray tube, without overheating the
anode **504**. This larger source may then be diffracted by a crystal
or other diffracting optic **506** to irradiate larger areas with
greater X-ray power than previously available. By application of
the Boettinger technique in reverse, as depicted in **Figure 12**,
10 the diffracted rays **508** from a large area transmission cathode
tube may be reduced in cross section and increased in power
density to values previously not readily available in the
laboratory. By application of the forward Boettinger technique
with an areal transmission photocathode X-ray tube, exceptionally
15 large beams of monochromatic radiation may be produced.

Although the invention has been described in relation to the
exemplary embodiment thereof, it will be understood by those
skilled in the art that other variations and modifications such
as, any X-ray system may be used with X-ray filters to
20 advantageously treat the X-ray spectrum to modify its properties
in ways well known to those skilled in the art, can be affected
in the preferred embodiment without detracting from the scope and
spirit of the invention as set forth in the claims.

ABSTRACT

5 The transmission cathode for X-ray generation is a device wherein an electrical current generated by a low voltage power supply produces an electron flow from the transmission cathode that is accelerated by a high voltage power supply towards an anode where X rays are emitted on impact. As the X rays are emitted, a primary beam passes through the cathode striking a sample placed outside the tube. The transmission cathode is
10 comprised of an electron emitter structure, preferably, an electron field emitter diode or thermionic emitter or a photoemitter or a nanotube or a pyroemitter or a piezoemitter, fabricated, preferably of elements of atomic numbers of 14 (silicon) or below, with electrically conductive components or
15 conductive mechanical structural components, preferably, conductive silicon or diamond or aluminum or beryllium metal, and non-conductive electrical insulators or non-conductive mechanical structural components, preferably, diamond or silicon dioxide or boron carbide. The transmission cathode is transmissive to those
20 X rays that freely flow through the transmission cathode.

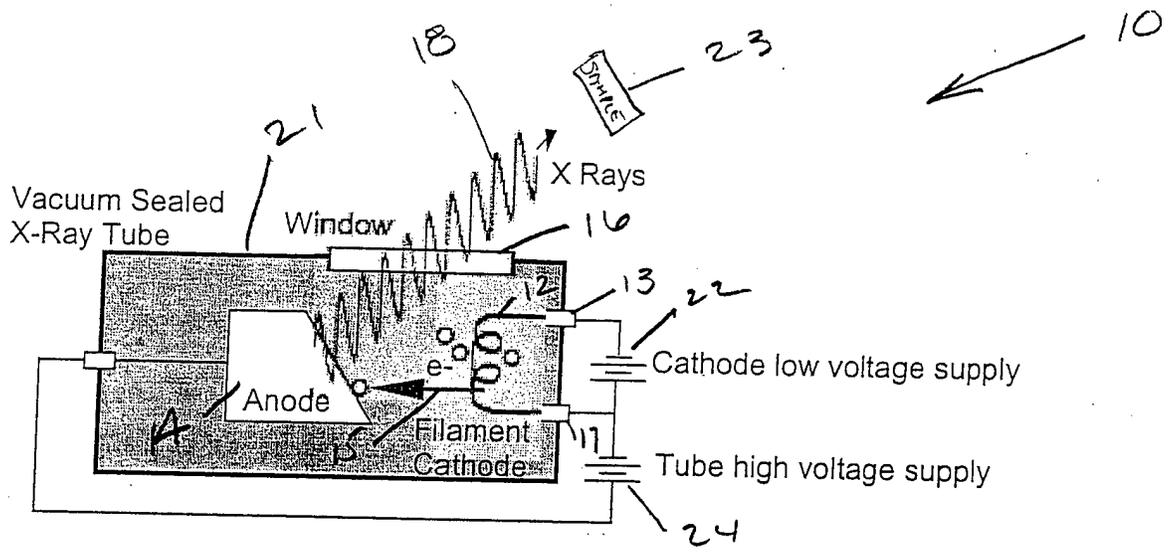


Figure 1a

PRIOR ART

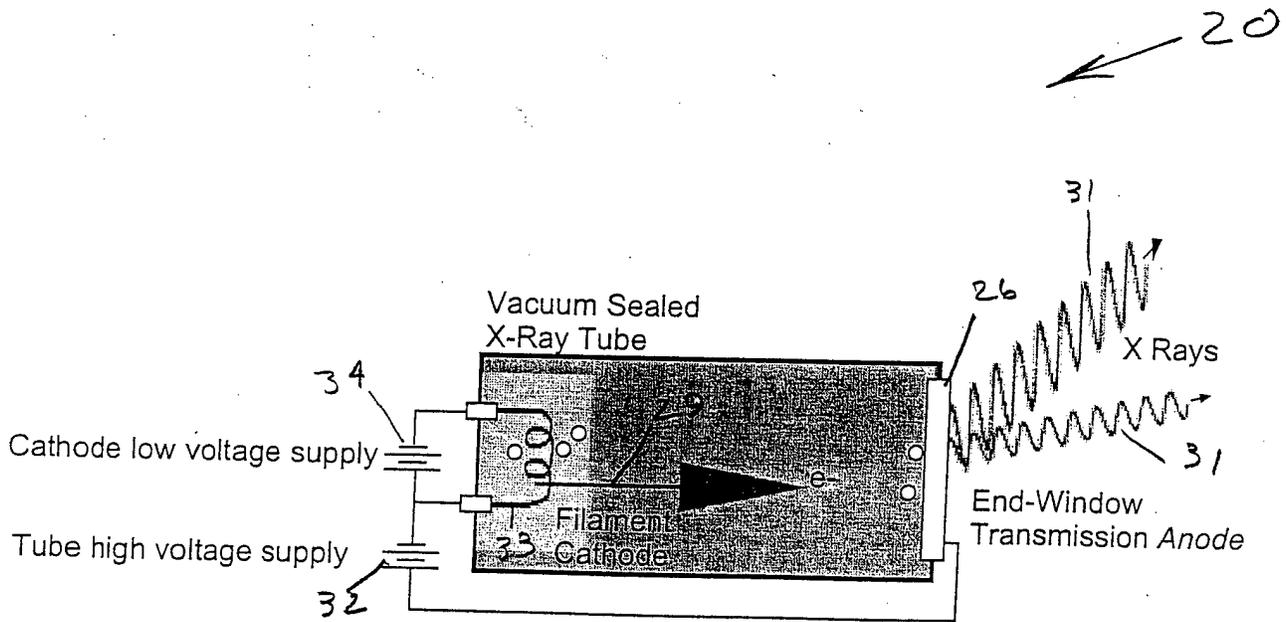


Figure 1b

PRIOR ART

PRIOR ART

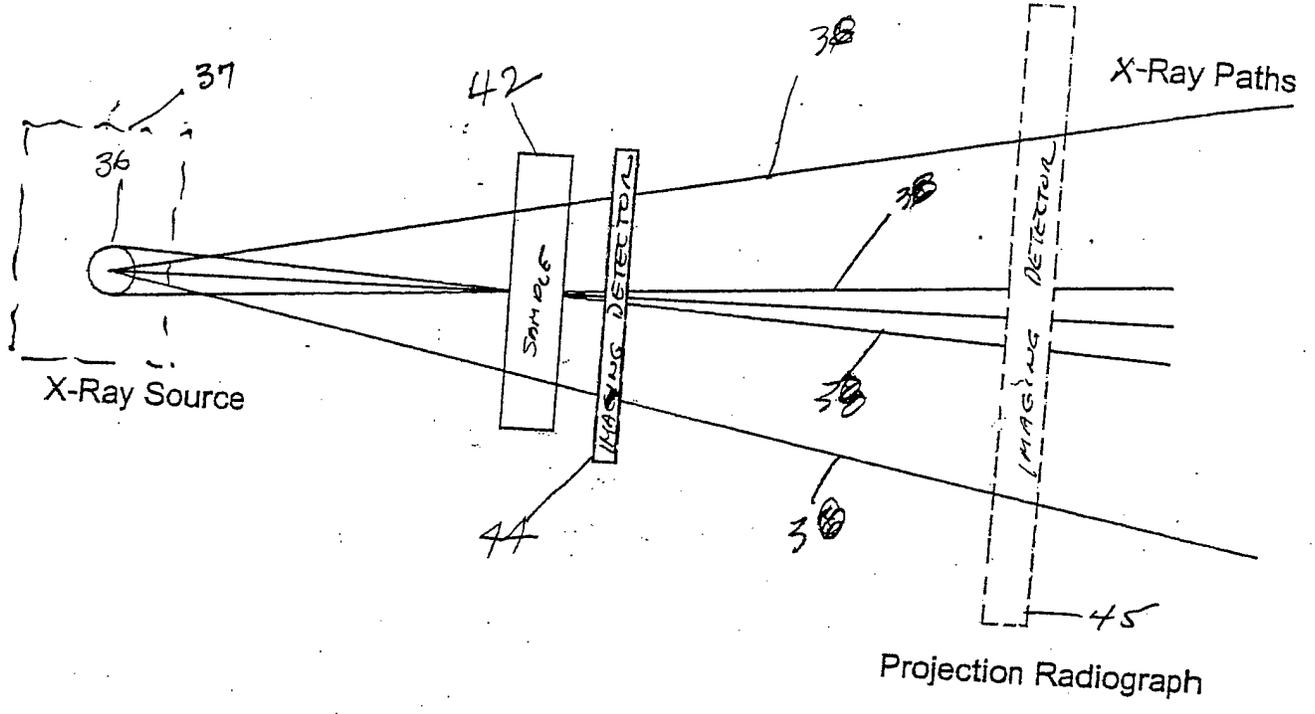


Figure 1c

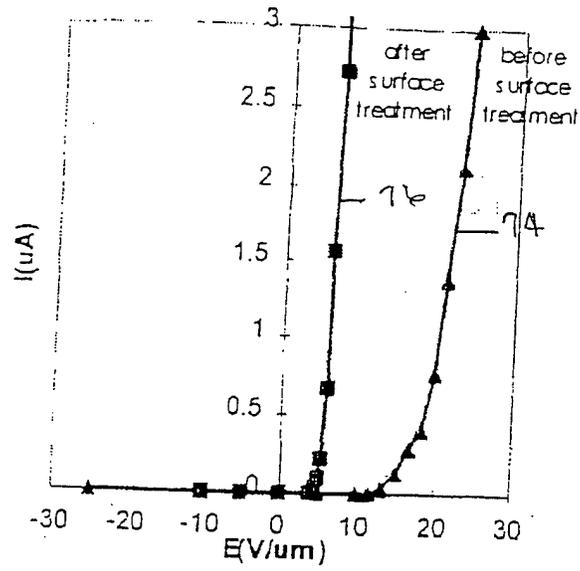


Figure 2d

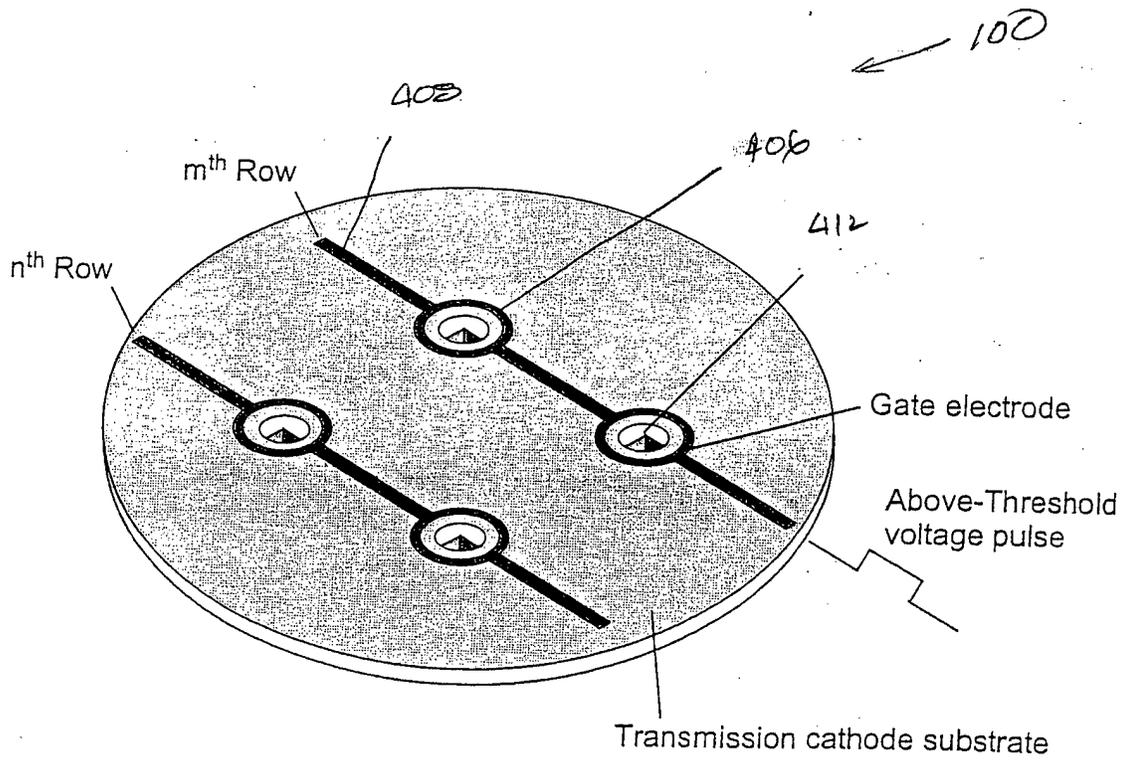


Figure 2e

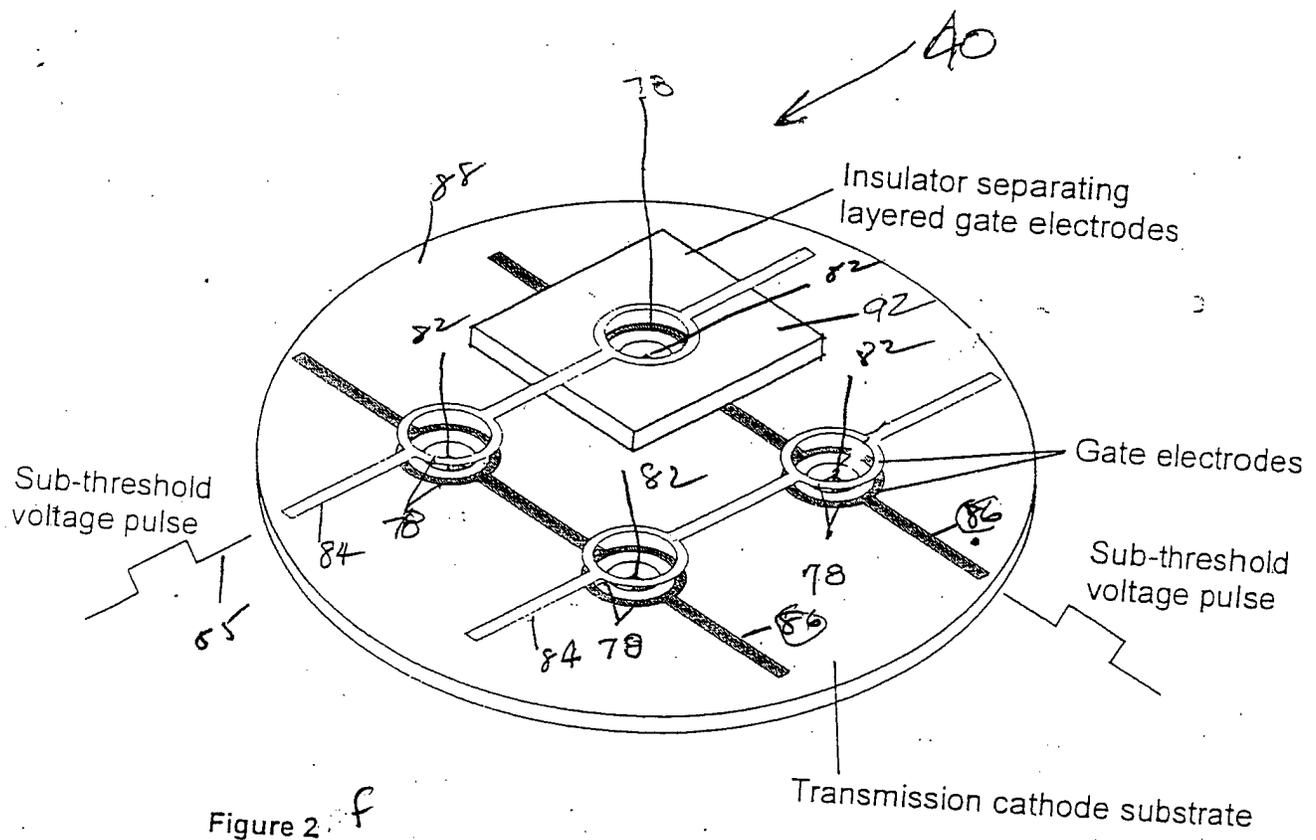


Figure 2 f

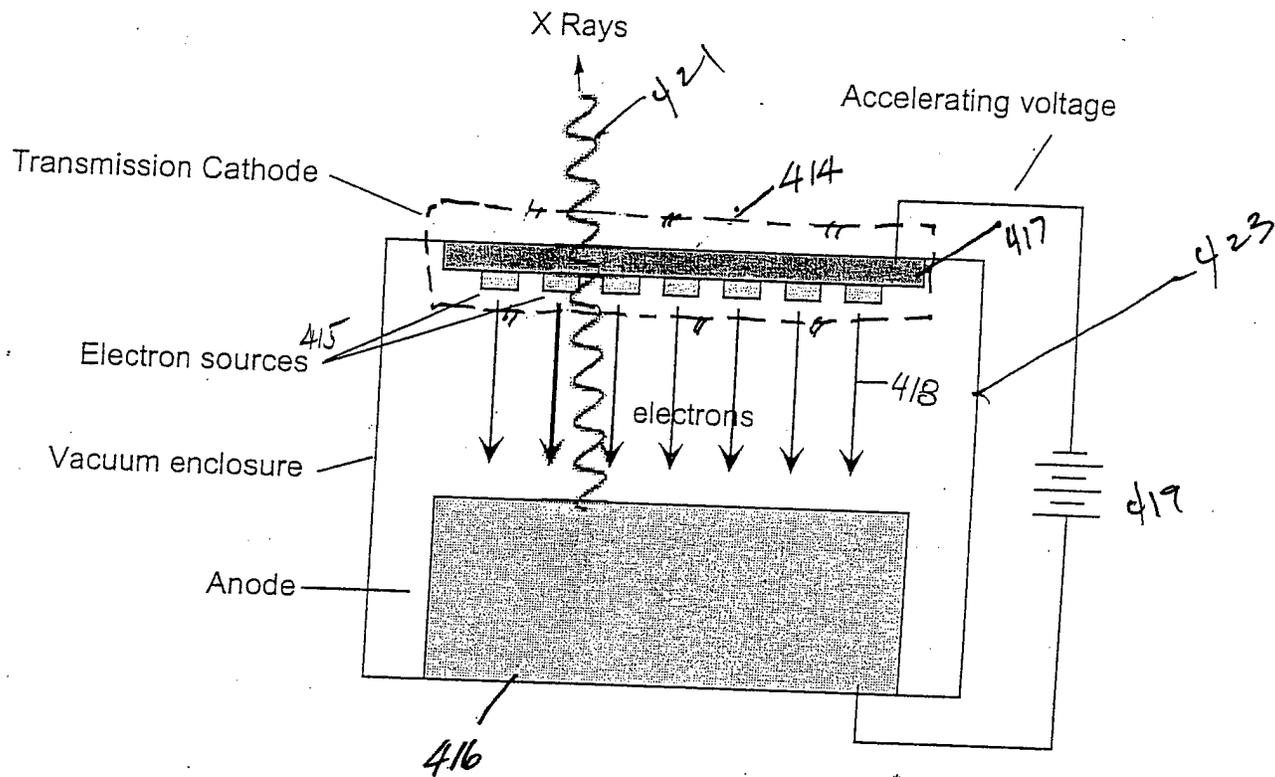


Figure 3

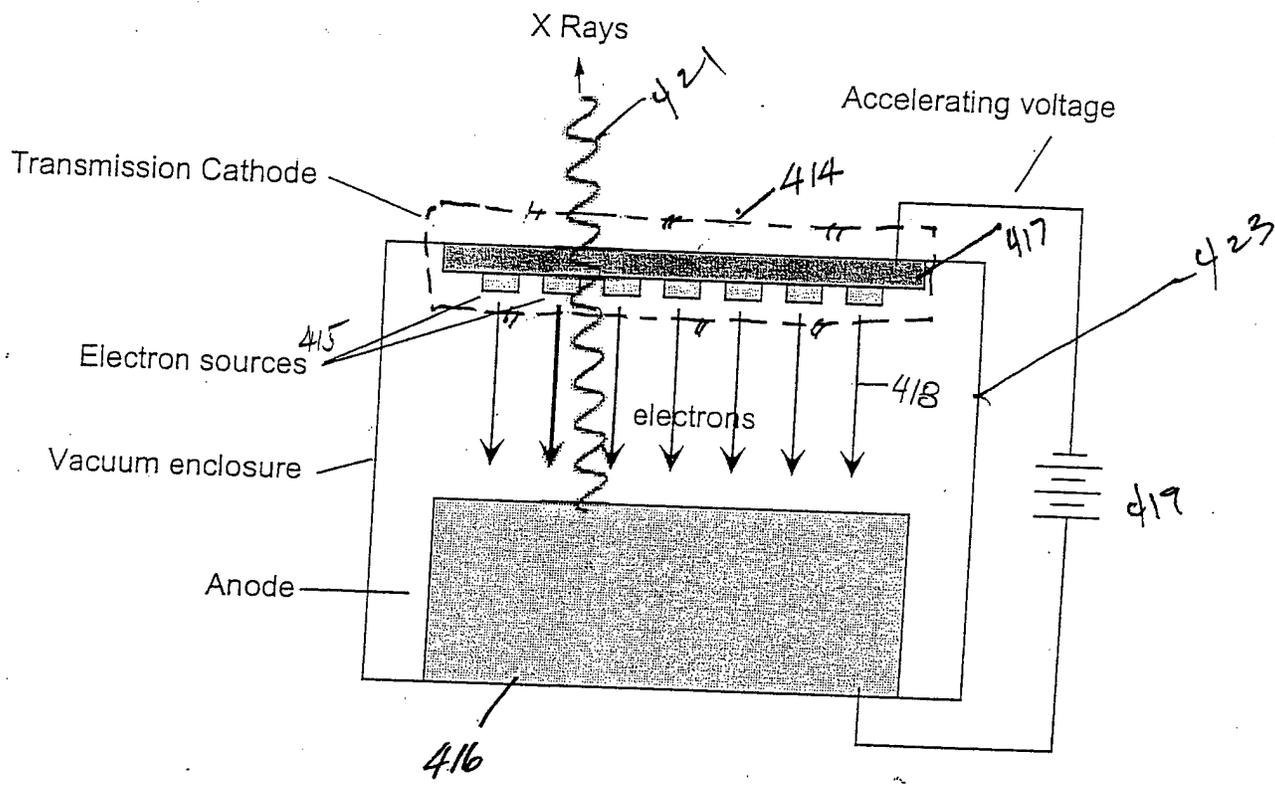


Figure 3

Duplicate

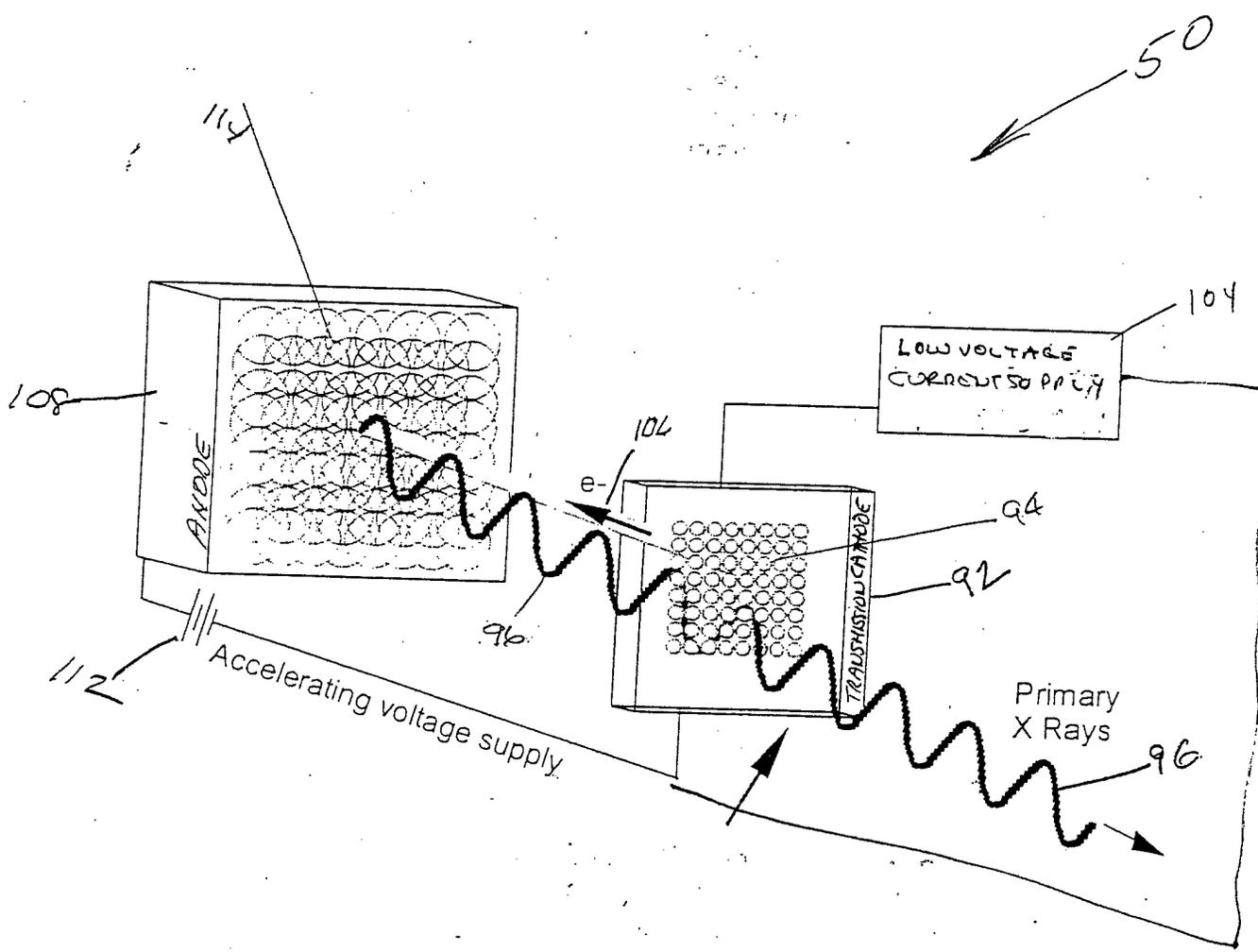


Figure 4

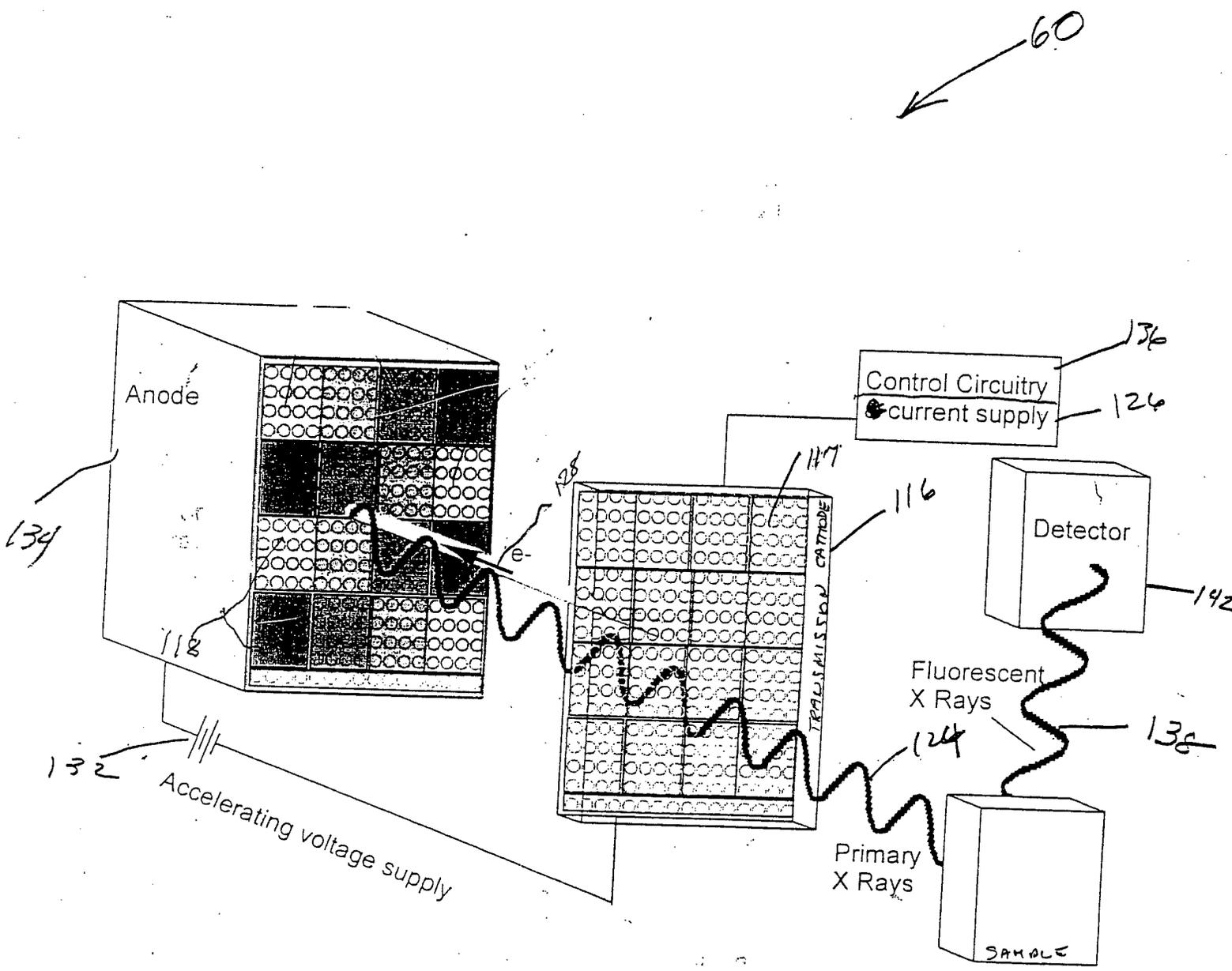


Figure a.

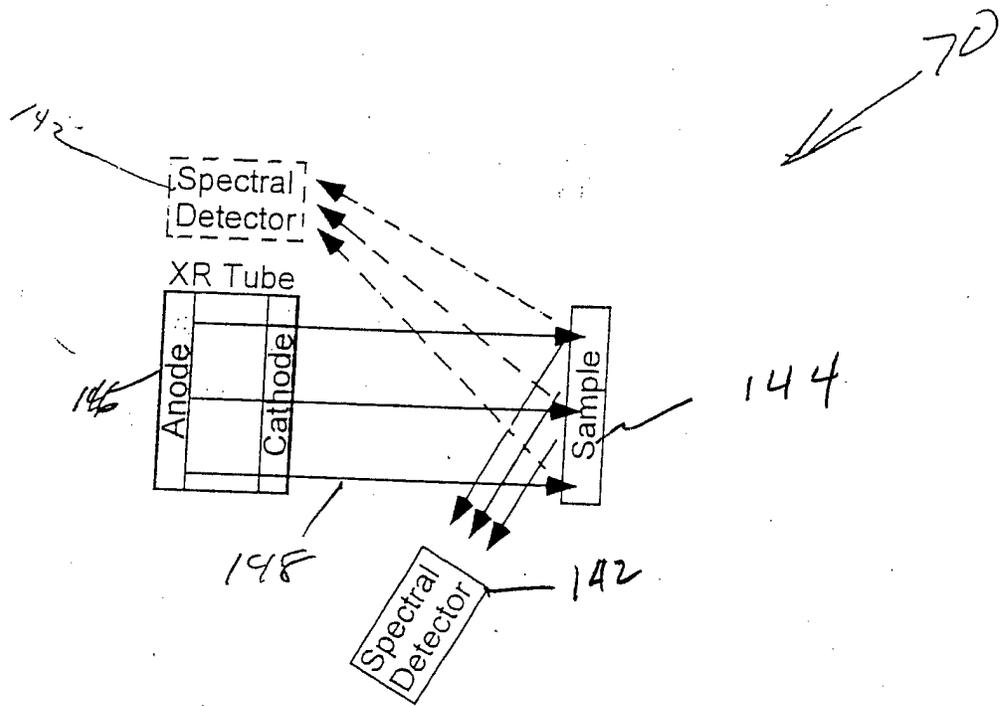


Figure 5b

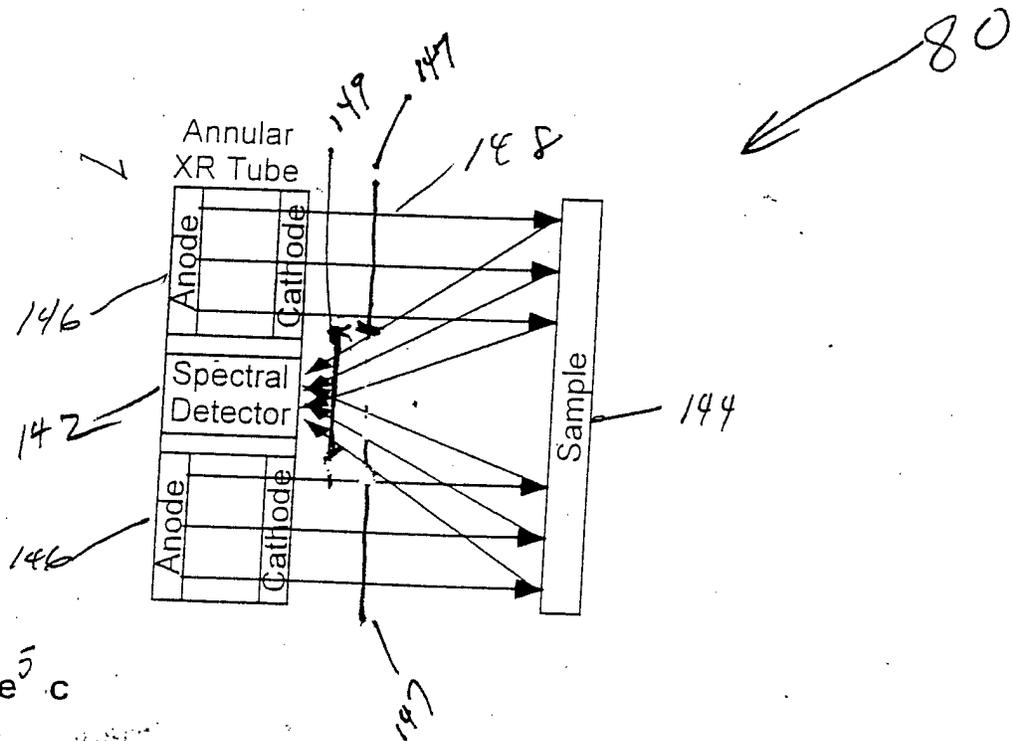


Figure 5c

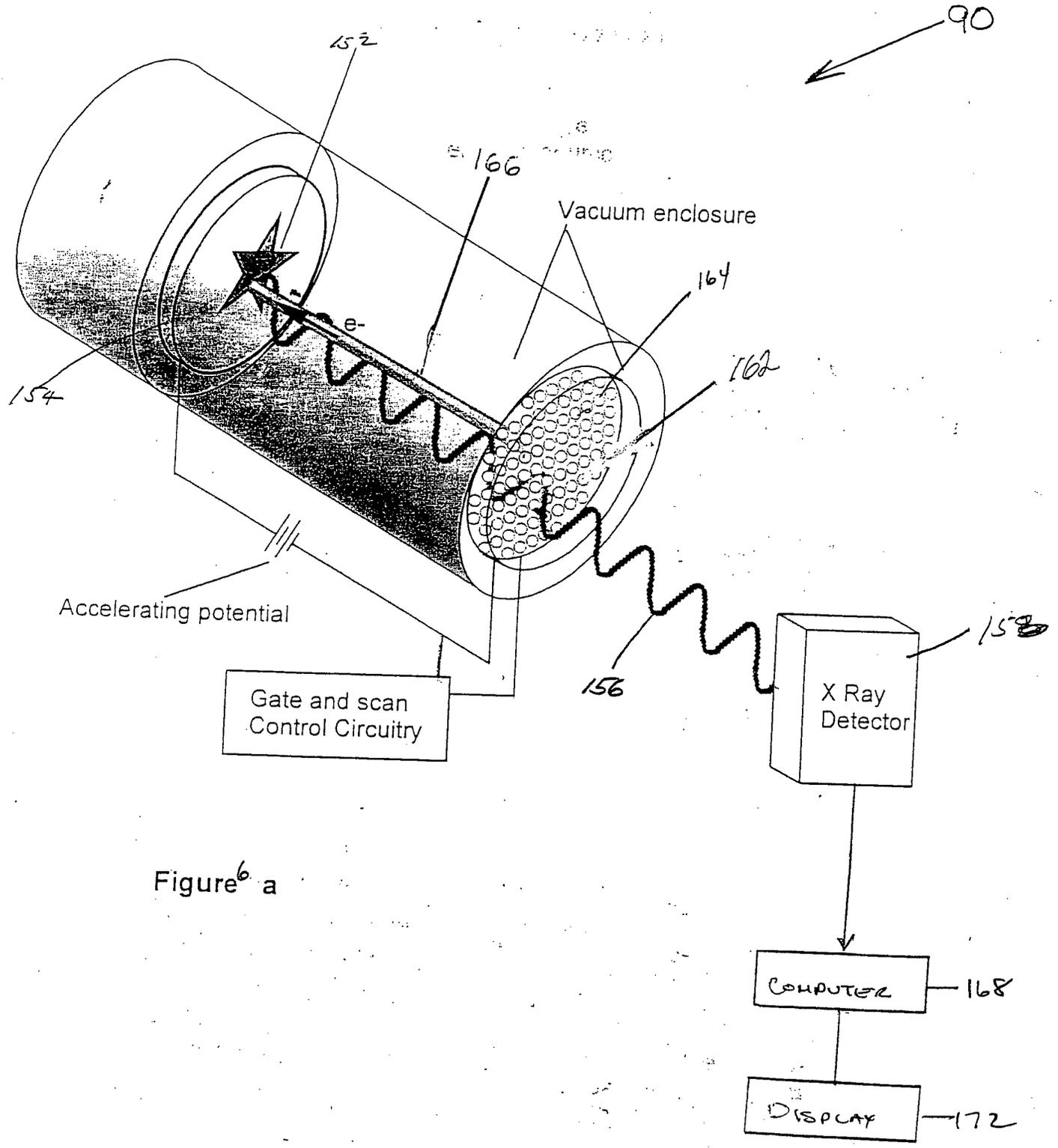


Figure 6 a

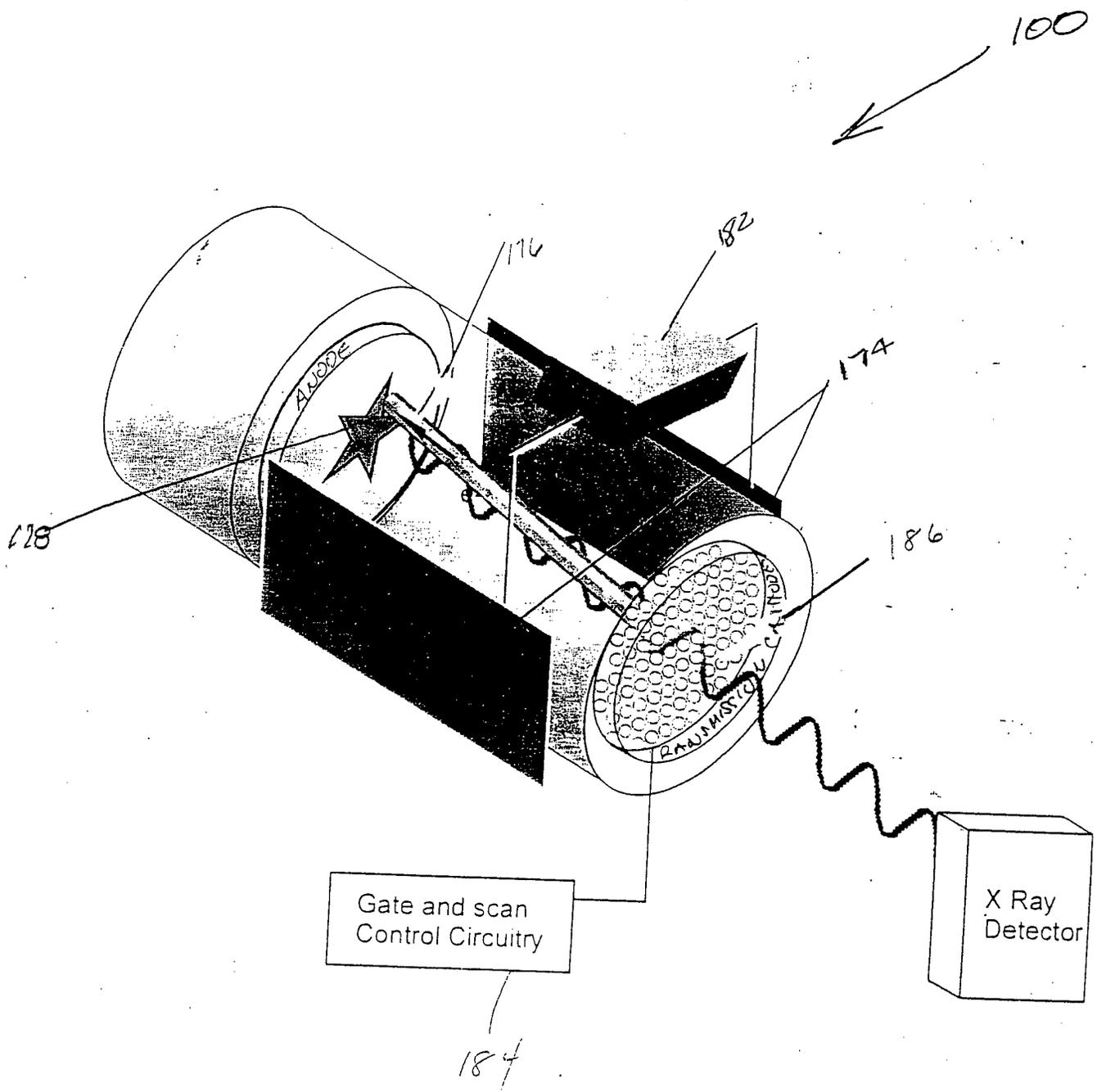


Figure 5b

110

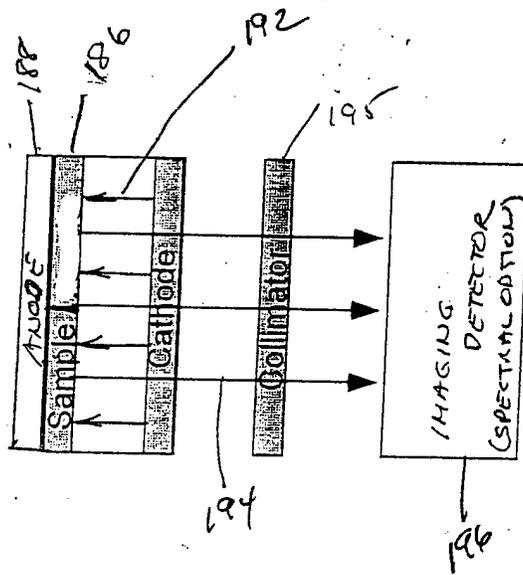


Figure 6c

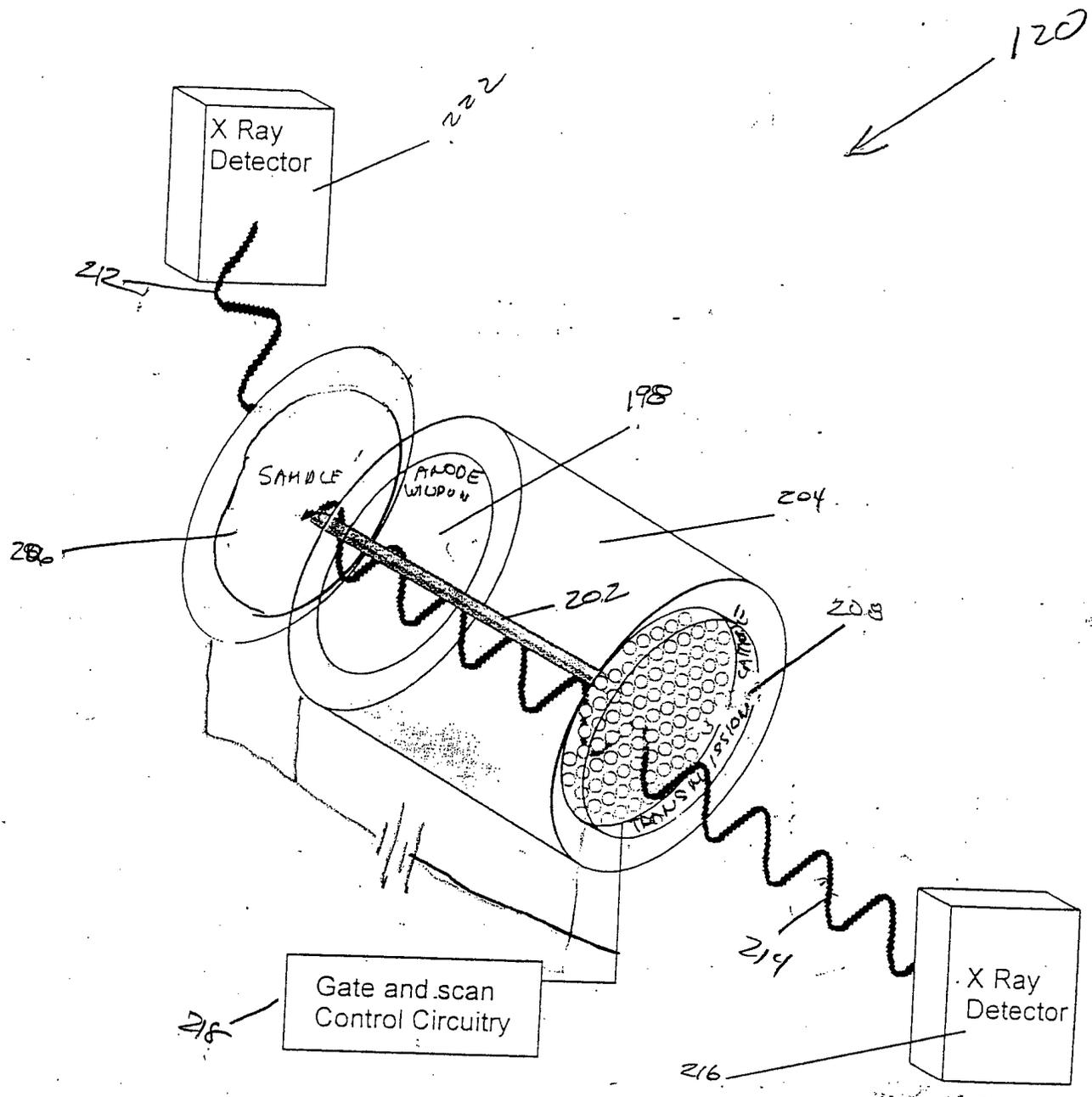


Figure 6d

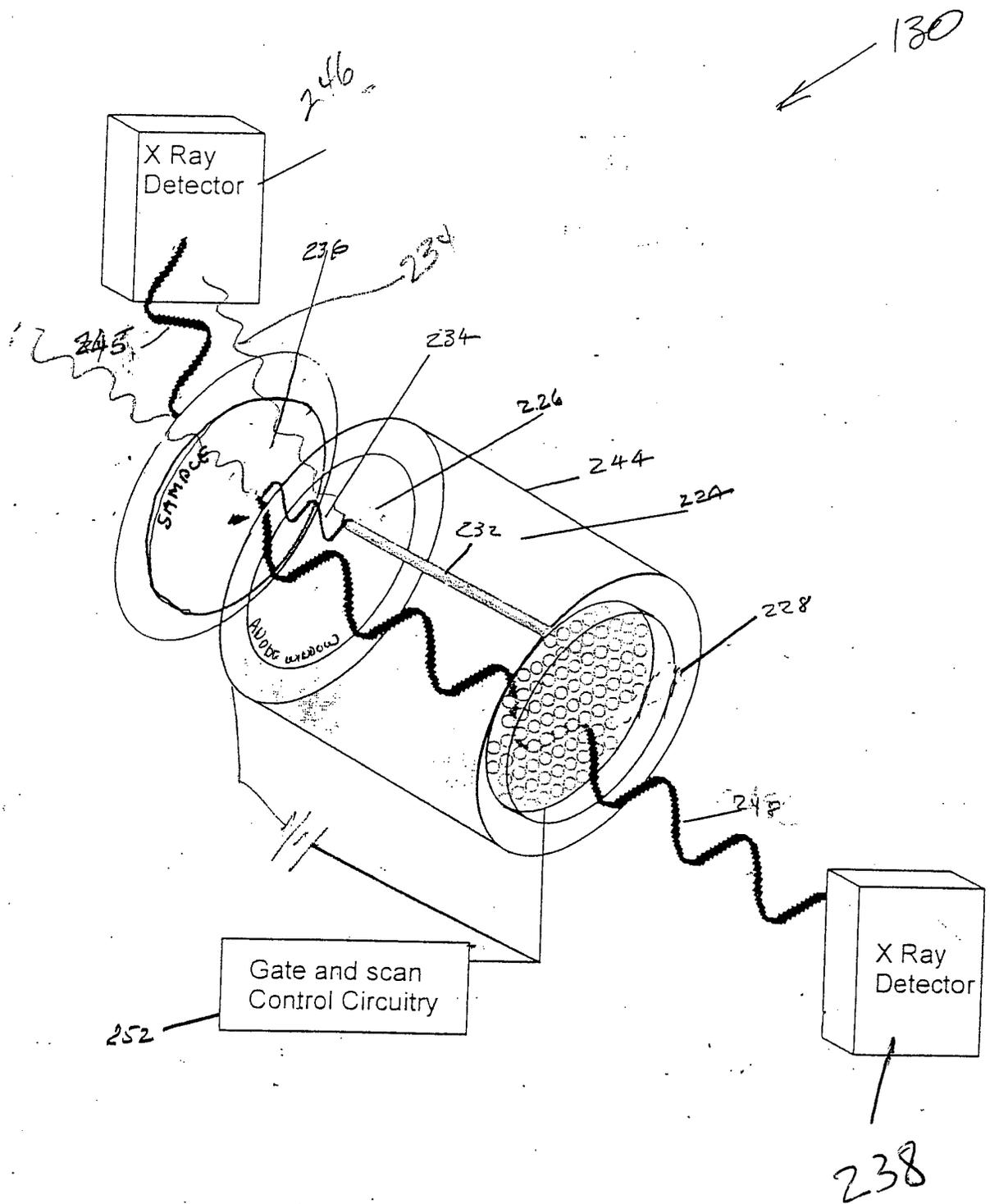


Figure 27

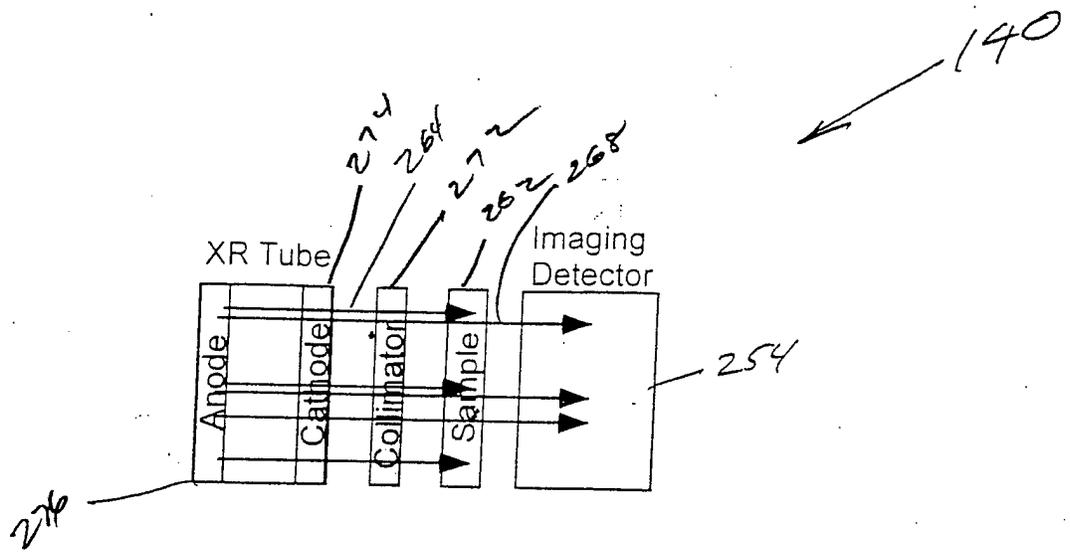


Figure 8a

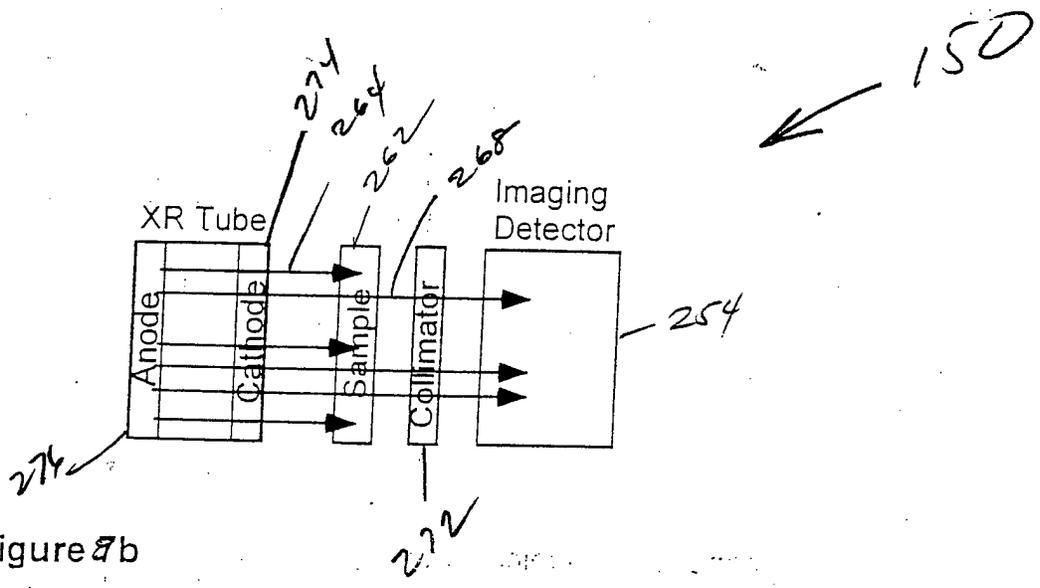


Figure 8b

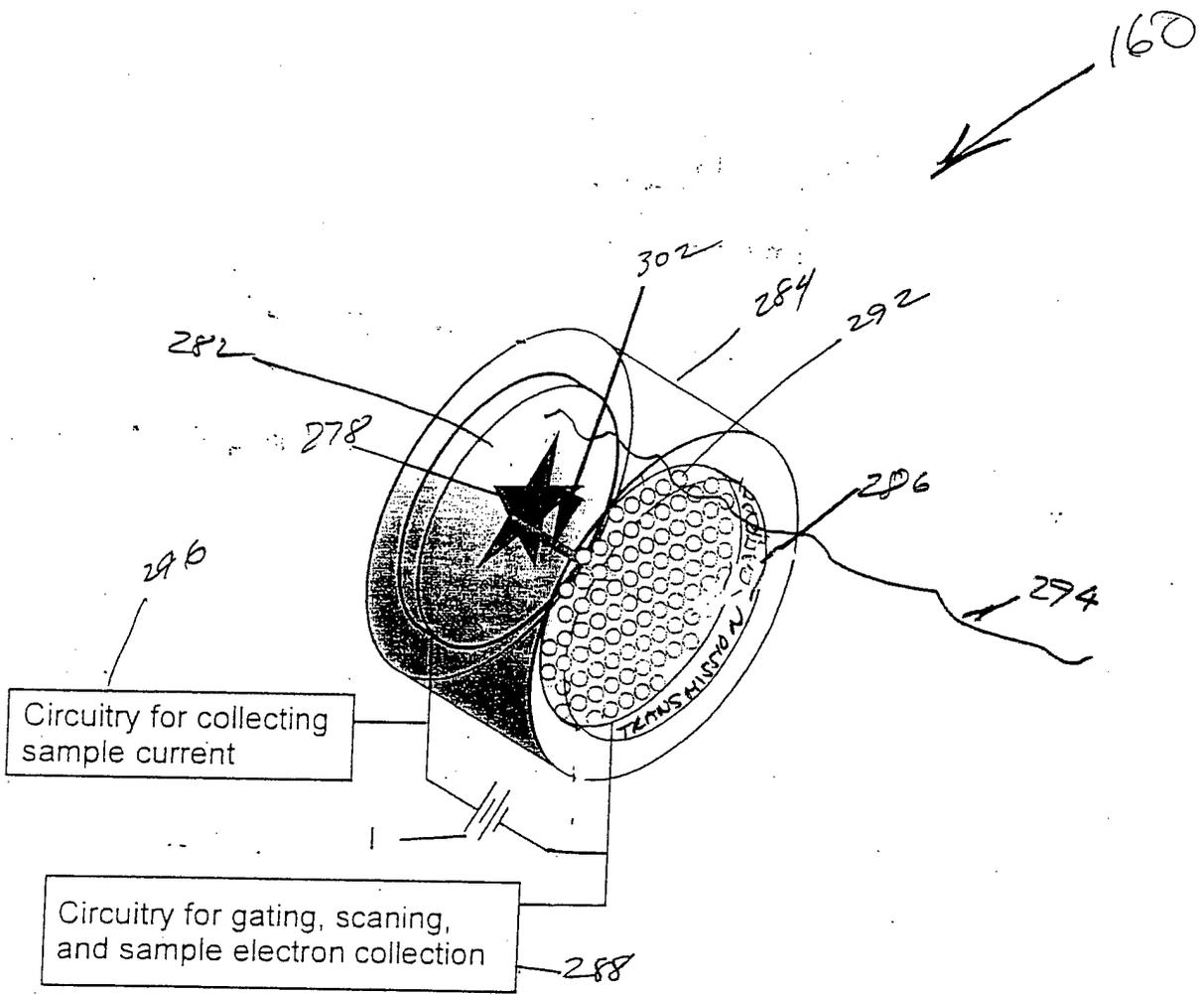


Figure 9a

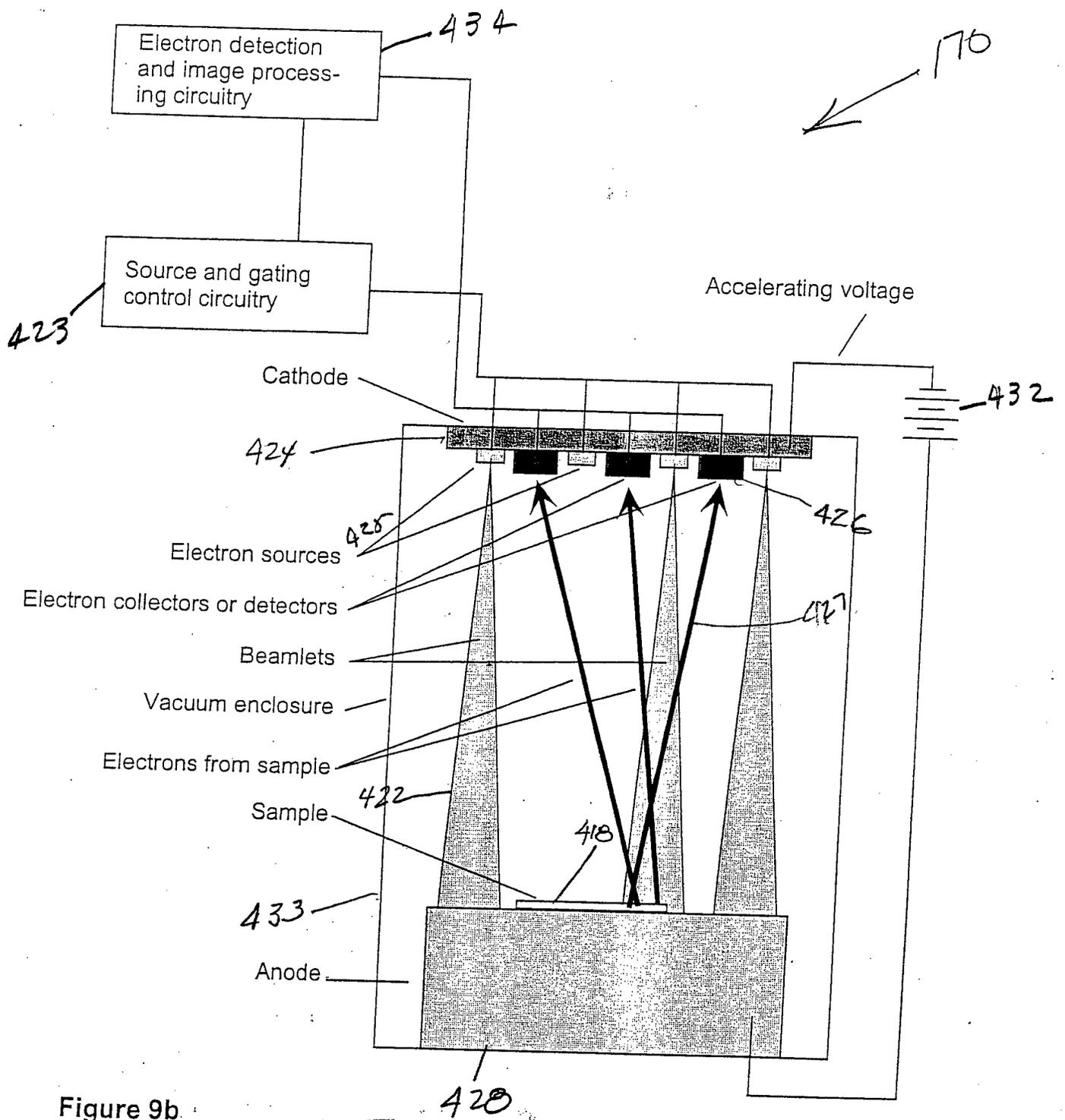


Figure 9b

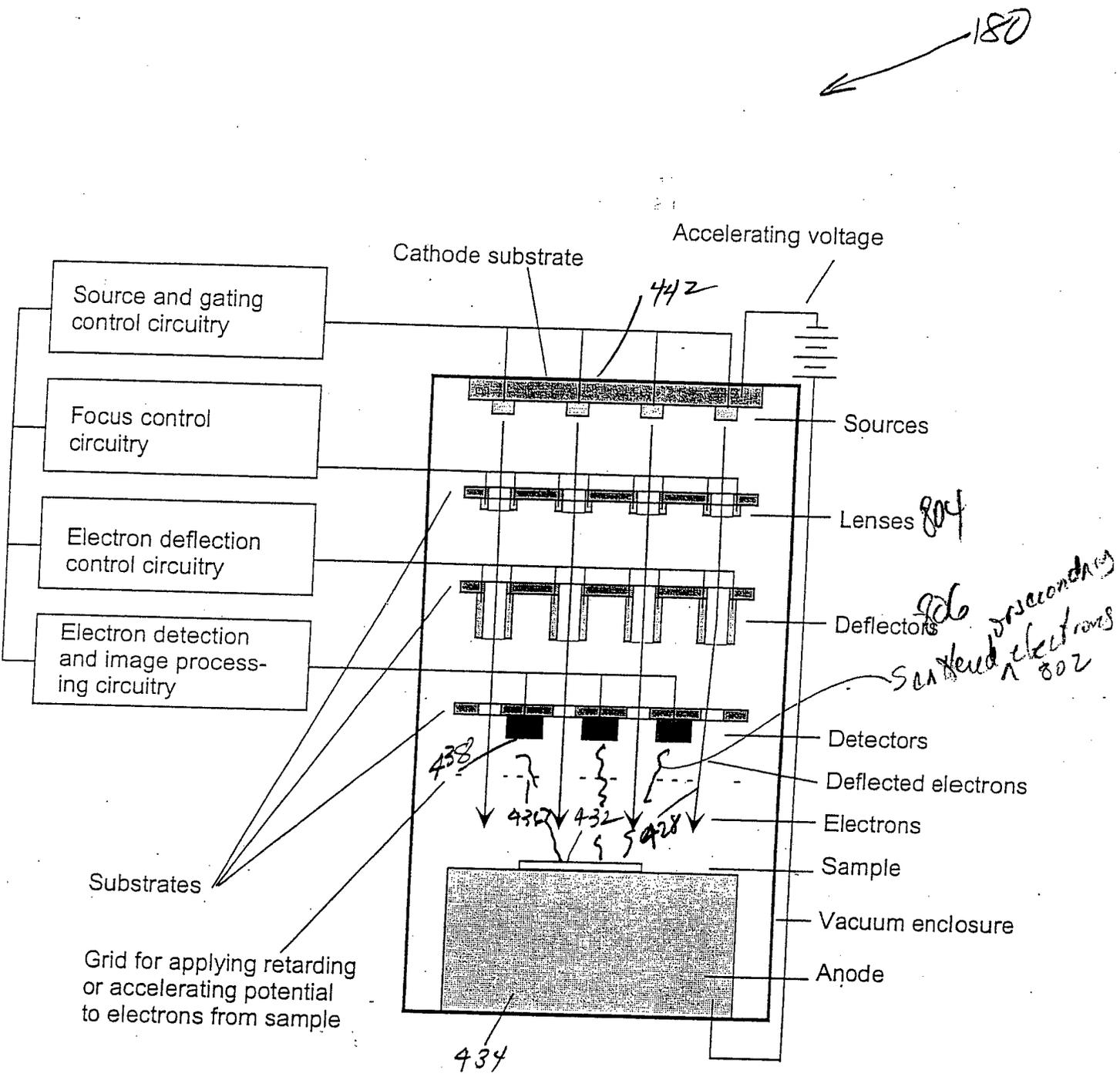


Figure 10

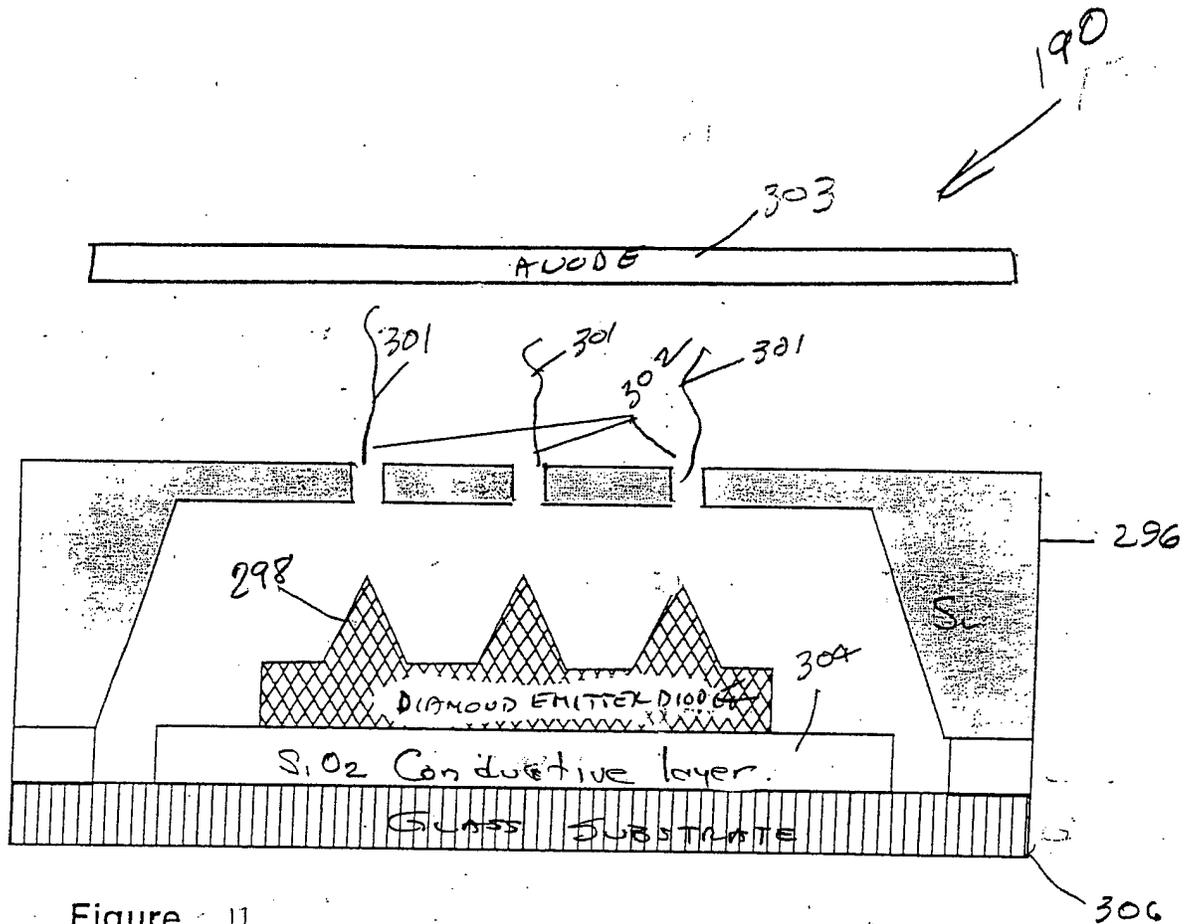


Figure 11

200

Transmission Cathode
X-Ray Tube

502

Diffractor
Input Beam

Diffractor
Output Beam

500

504

Asymmetric Diffractor

506

Fig 12

